Objective and Motivation

A recognized side effect of prolonged microgravity (μg) exposure is visual impairment and intracranial pressure (VIP) syndrome [1]. Though there is limited medical understanding of this phenomenon, it is hypothesized that cephalic shift of the cerebrospinal fluid (CSF) and blood in μg may be a contributor. Computational models can be used to provide insight into the origins of VIP [1, 2]. In order to further investigate this phenomenon, NASA’s Digital Astronaut Project (DAP), in collaboration with some of the world’s leading experts in ocular biomechanics, is developing an integrated fluid physics-based computational model of the human cardiovascular system (CVS). This poster summarizes our current progress on the development and testing of an integrated computational model of CVS and CNS based on the whole-body lumped-parameter (LP) model presented by Lakin et al. (2003) [3]. These models will provide unique capabilities to give insight into the physiological changes that cannot be directly measured (e.g., changes in ICP), and to help answer questions related to the following research knowledge gaps:

VIP1: We do not know the etiological mechanisms and contributing risk factors for occular structural and functional changes seen in-flight and post-flight.

VIP2: How are fluids redistributed in flight?

VIP3: We need to identify preventive and treatment countermeasures (CMs) to mitigate changes in ocular structure and function and intracranial pressure during spaceflight.

Methods

We reproduced the steady-state 16-compartment whole-body LP model presented by Lakin et al. [3] (Figure 1). The general structure of the model:

- Includes blood, cerebrospinal fluid (CSF), tissue, interstitial fluid, pulmonary circulation and organs
- Captures direct flow between compartments, as well as transfer of fluid between capillaries and tissue by filtration
- Includes compliant interactions between adjacent compartments
- Incorporates functions to allow the inclusion of the lymphatic system and the sympathetic nervous system (SNS) functions
- Includes a series of 13 differential equations to describe the pressure dynamics of the system in accordance with the laws of conservation

\[ \text{flow in} = \text{flow out} = \text{rate of volume change} \]  
(1)

- Formulates the governing equations in a matrix form:

\[ [c] \cdot \frac{\partial [e]}{\partial t} + [e] \cdot \frac{\partial [P]}{\partial t} = [0] \]  
(2)

- Incorporates lymphatic, intracranial, and SNS through forcing and regulatory mechanisms

In addition, the following assumptions are applied:

- All fluids are assumed to be incompressible and isotermal
- Pressure-driven flows are laminar and governed by the hydrodynamic equation:

\[ Q_i = \frac{P_i - P_j}{R_{ij}} = \frac{1}{C_{ij}}(P_i - P_j) \]  
(3)

- Fluid filtration between the capillary and the interstitial spaces is governed by the Starling-Landin equation:

\[ \text{Filtration} = K_{nf}(P_c - P_i) - n_k(\Delta P - n_i) \]  
(4)

- Compliance between compartments depends on the change in pressure differences between compartments in the form of:

\[ \frac{\partial r_{ij}}{\partial t} = C_{ij} \frac{\frac{\partial (P_c - P_i)}{\partial t}}{C_{ij}} \]  
(5)

- Revises the Kellie-Monroe Doctrine in order to take into account the influence of extra-cranial physiology on ICP dynamics

- Hydrostatic pressure variation can be approximated through an ad hoc variation of resistances in the upper and lower portions of the body

\[ \text{Legend:} \]
- \( R_i \): resistance between the two compartments
- \( P_i \): capillary pressure
- \( Q_i \): flow from compartment \( i \) to compartment \( j \)
- \( r_{ij} \): compliance coefficient

Verification and Validation

The initial verification test challenged the model in a time-dependent mode by specifying steady-state values that were offset by 10% from Lakin et al.’s [3] mean values to perturb the system. Since the system returned to the baseline mean values, our model successfully conserves all conservation parameters.

In addition, we performed two validation cases as outlined by Lakin et al. [3] to examine the dynamic behavior of the model for the situations of:

- Pulsatile heart flow, and
- Postural change

Verification and Validation

References


Results and Discussions

The model successfully simulated a pulsatile cardiac cycle that was comparable to [3]. As can be seen in Figure 2, there are minor discrepancies in the period and amplitude of our prediction of heart outflow and Lakin et al.’s function, as digitized from the paper. However, when compared with literature values [4], our simulated systolic and diastolic pressures in the central and intracranial arteries were within physiological limits of 120/80 mmHg and 100/65, respectively, as presented in Figure 3. We therefore considered our model’s response to be satisfactory.

Forward Work

In order to leverage this model as a foundation for an integrated systems model to simulate the CNS and CVS for VIP research, we will:

- Formally incorporate hydrostatic pressure variation into the matrix equation
- Modify system parameters such as tissue and flow properties, flowrates and pressures to reflect the most current VIP research and to define a reasonable physiological envelope that encompasses the astronaut corps
- Analyze the model via sensitivity studies to locate most significant parameters
- Test the model against and train the model with independent studies in postural change, head-down tilt and μg to develop and validate regulatory functions that appropriately capture the observed fluid redistribution
- Ascertain trend and characteristic ranges of output variables for use by the CNS and eye models, including fluid redistribution and cranial blood flow in μg