

DEVELOPMENT OF THE NASA DIGITAL ASTRONAUT PROJECT MUSCLE MODEL

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BACKGROUND

NASA's Digital Astronaut Project (DAP) Vision

The Digital Astronaut Project implements well-validated computational models to predict and assess spaceflight health and performance risks, and enhance countermeasure development

HRP Risks/Gaps Addressed by This Effort

- Risk of Muscle Atrophy:** Impaired performance due to reduced muscle mass, strength and endurance
- M2 - Characterize in-flight and post-flight muscle performance**
- M7 - Develop the most efficient exercise program for the maintenance of muscle fitness**
- M24 - Characterize the time course of changes in muscle protein turnover, muscle mass and function during long duration space flight**

Musculoskeletal Modeling Objectives

Use an integrated musculoskeletal modeling approach to support the bone remodeling model efforts and provide muscle performance prediction capabilities:

- Provide bone loading information from biomechanical models of exercise that incorporate muscles that reflect spaceflight atrophy
- Develop algorithms which equate mechanical stimulus from in-flight exercise to muscle maintenance
- Predict the minimal amount of stimulus needed to maintain required performance levels
- Predict if the stimulus be achieved by performing in-flight exercise on the available exercise devices
- Predict task performance after a specified time in space
- Predict the minimum amount of muscle strength and power to perform a task

MUSCLE MODEL COMPONENTS

Tendon Force - Muscle Force Equilibrium Equation

$$F_T = F_{M0} = (a_f l_f v_f + f_{PE}) \cos \alpha$$

F_T = Tendon force vs strain

F_{M0} = Maximum isometric force

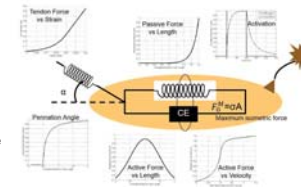
a_f = Neuromuscular activation

l_f = Active force vs length curve

f_{PE} = Active force vs velocity curve

f_{PE} = Passive force vs length curve

α = Pennation angle



UNCERTAINTY, SENSITIVITY AND VALIDATION ANALYSES

Objectives

- Use simplified exercise models to gain a sufficient understanding of the OpenSim modeling environment and to determine how to augment OpenSim in order to model spaceflight induced muscle atrophy

Methods

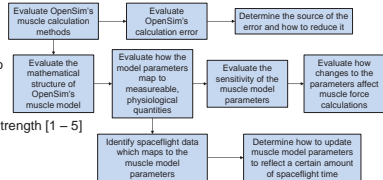
- OpenSim models of exercises used to assess post-flight strength [1 - 5]
 - Isometric and isokinetic plantar flexion exercises [6 - 9]
 - Isometric and isokinetic knee flexion and extension exercises [10]
 - Leg press exercise to obtain maximum explosive power [11]
- Kinematics input files specify joint angles and kinetics input files specify joint torques/ground reaction forces
- Muscle excitations obtained with a Computed Muscle Control analysis
- Muscle forces calculated with a forward dynamics analysis
- Analyses performed:
 - Calculated joint torques/ground reaction forces compared to prescribed values to find calculation error
 - Muscle parameters adjusted systematically to determine sensitivity
 - Muscle parameters modified to reflect spaceflight data in order to quantitatively compare preflight and post-flight conditions

Results

- Calculation error typically ranged from 1 - 10%, submaximal cases tended to be higher
 - In some cases, calculation error is larger than the differences due to spaceflight and must be reduced for meaningful comparison of 1g to spaceflight conditions
- Tendon slack length and optimal fiber length identified as the most sensitive model parameters
 - Allows prioritization of parameters when addressing parameters for which data is lacking
- Post-flight predictions when changing only the maximum isometric force parameter was successful for isometric and low velocity isokinetic strength predictions, but not for high velocity isokinetic cases
 - Spaceflight data suggests that a reduction in force cannot be explained by reduction in volume alone
 - Neuromotor control, morphology, specific tension, stiffness properties, etc. may also be important
 - These preliminary results suggest that they need to be accounted for in the model

Future Work

- Complete leg press analysis, with particular focus on error due to unknown kinematics
- Determine and develop strategies to minimize the main sources of calculation error in OpenSim
- Take further advantage of the OpenSim optimization methodologies and capabilities
- Complete sensitivity analysis with parameters that are constant across all muscles
- Develop ranges for muscle model parameters which reflect
 - Uncertainty due to individuality
 - Change due to spaceflight as a function of
 - Time in space
 - Level of in-flight exercise performed
- Explore alternative optimization methods for fitting parameters to address [12]:
 - The interdependency of the parameters
 - The lack of quantitative data for all parameters



OpenSim plantar flexion model



OpenSim knee flexion/extension model

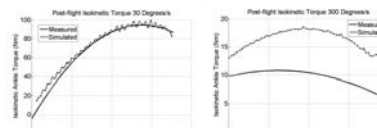
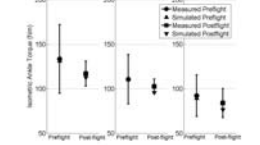


OpenSim leg press model



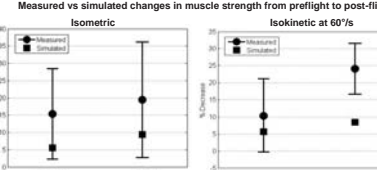
Plantar flexion analysis results

Measured vs simulated comparisons of preflight and post-flight strength measurements



Knee flexion/extension analysis results

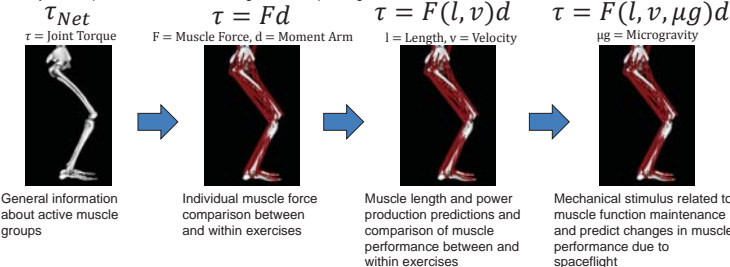
Measured vs simulated changes in muscle strength from preflight to post-flight



OPERATIONAL CONCEPT

Support Advanced Exercise Countermeasures Project

Advance from prediction of joint torque to muscle force to muscle force as a function of muscle length and velocity to incorporation of muscular changes due to spaceflight

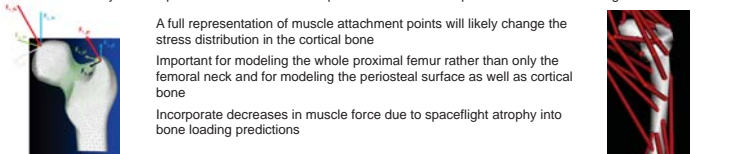


Inform questions such as:

- How does muscle performance differ between different exercise devices, types of exercises and exercise configurations?
- Does the limited volume and power requirements affect the muscle forces generated during prescribed exercises?
- Does that affect the ability of the countermeasure device to maintain muscle performance?
- How does that affect the astronaut's ability to perform required tasks?

Support Bone Remodeling Modeling Efforts

Increase the fidelity of the input force to the FEM which provides bone strain input to the bone remodeling model



MUSCLE MODEL CONCEPT

DAP Muscle Model Concept

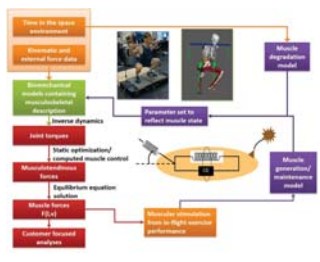
Version 1.0 (Target completion, 9/2016) model input includes time spent in space and qualitative level of exercise use (low, average, high)

The model uses spaceflight and Earth based analog data to perform a parameter fit for the OpenSim muscle model parameters

Model output is an OpenSim muscle model parameter set that reflects the state of the muscle after the specified amount of time in space and exercise use

Version 2.0 (Target completion, 9/2019) based upon two functions:

- 1) Muscle degradation vs. time in microgravity
- 2) Muscle generation/maintenance as a function of muscle contraction and stretch during the mission



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[1] S. R. Hamner, A. Seth, and S. L. Delp. "Muscle contributions to propulsion and support during running." *J. Biomech.*, vol. 43, no. 14, pp. 2709-2716, Jan. 2010.

[2] D. G. Thelen and F. C. Anderson. "Using computed muscle control to generate forward dynamic simulations of human walking from experimental data." *J. Biomech.*, vol. 39, no. 6, pp. 1107-1115, Jan. 2006.

[3] D. G. Thelen, F. C. Anderson, and S. L. Delp. "Generating dynamic simulations of movement using computed muscle control." *J. Biomech.*, vol. 36, no. 3, pp. 321-328, Mar. 2003.

[4] E. M. Arnold, S. R. Ward, R. L. Lieber, and S. L. Delp. "A model of the lower limb for analysis of human movement." *Ann. Biomed. Eng.*, vol. 38, no. 2, pp. 269-279, Feb. 2010.

[5] M. Millard, T. Uchida, A. Seth, and S. L. Delp. "Flexing computational muscle: modeling and simulation of musculoskeletal dynamics." *J. Biomech. Eng.*, vol. 135, p. 021005, 2013.

[6] S. Trappe, D. Costill, P. Gallagher, A. Cree, J. R. Peters, H. Evans, D. A. Riley, and R. H. Fitts. "Exercise in space: human skeletal muscle after 6 months aboard the International Space Station." *J. Appl. Physiol.*, vol. 106, no. 4, pp. 1159-68, Apr. 2009.

[7] S. W. Trappe, T. A. Trappe, G. A. Lee, and D. L. Costill. "Calf muscle strength in humans." *Int. J. Sports Med.*, vol. 22, pp. 186-191, 2001.

[8] M. F. Bobbert and G. J. Van Ingen Schenau. "Isokinetic plantar flexion: Experimental results and model calculations." *J. Biomech.*, vol. 23, pp. 105-119, 1990.

[9] M. Y. Pang and M. K. Mak. "Influence of contraction type, speed, and joint angle on ankle muscle weakness in Parkinson's disease: Implications for rehabilitation." *Arch. Phys. Med. Rehabil.*, vol. 93, pp. 2352-2359, 2012.

[10] R. Gopalakrishnan, K. O. Genc, A. J. Rice, S. M. C. Lee, H. J. Evans, C. C. Maender, H. Bastian, and P. R. Cavanagh. "Muscle Volume, Strength, Endurance, and Exercise Loads During 6-Month Missions in Space." *Aviat. Space. Environ. Med.*, vol. 81, no. 2, pp. 91-104, Feb. 2010.

[11] G. Antonutto, C. Capelli, M. Girasole, P. Zamparo, and P. E. di Prampero. "Effects of microgravity on maximal power of lower limbs during very short efforts in humans." *J. Appl. Physiol.*, vol. 86, no. 1, pp. 85-92, Jan. 1999.

[12] E. Balas-Canto and J. Bangs. "AMIGO: A model identification toolbox based on global optimization and its applications in biosystems." *Comput. Appl. Biotechnol.*, vol. 11, no. 1, pp. 132-7, 2010.

REFERENCES

PARTNERS

