Cardiovascular Adaptations to Long Duration Head-Down Tilt Bed Rest

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INTRODUCTION: Orthostatic hypotension is a serious risk for crewmembers returning from spaceflight. Numerous cardiovascular mechanisms have been proposed to account for this problem, including vascular and cardiac dysfunction, which we studied during bed rest. METHODS: Thirteen subjects were studied before and during bed rest. Statistical analysis was limited to the first 49-60 days of bed rest, and compared to pre-bed rest data. Ultrasound data were collected on vascular and cardiac structure and function. Tilt testing was conducted for 30 minutes or until presyncopal symptoms intervened. RESULTS: Plasma volume was significantly reduced by day 7 of bed rest. Flow-mediated dilation in the leg was significantly increased at bed rest day 49. Arterial responses to nitroglycerin differed in the arm and leg, but did not change as a result of bed rest. Intimal-medial thickness markedly decreased at bed rest days 21, 35 and 49. Several cardiac functional parameters including isovolumic relaxation time, ejection time and myocardial performance index were significantly increased (indicating a decrease in cardiac function) during bed rest. There was a trend for decreased orthostatic tolerance following 60 days of bed rest. DISCUSSION: These data suggest that 6° head-down tilt bed rest alters cardiovascular structure and function in a pattern similar to short duration spaceflight. Additionally, the vascular alterations are primarily seen in the lower body, while vessels of the upper body are unaffected.

KEY WORDS: spaceflight, orthostatic intolerance, hypotension, fluid-shift, plasma volume
INTRODUCTION

Spaceflight provokes numerous untoward effects on the cardiovascular system. These effects have been shown in spaceflight studies (1), bed rest analog studies (20) and animal studies (18). Post-spaceflight orthostatic hypotension has been the subject of intense study during the last 20 years, both during spaceflight and head-down tilt bed rest investigations. This problem appears to develop from a series of in-flight cardiovascular changes including a relative hypovolemia, initiated by the cephalad fluid shift and a lack of arterial baroreceptor input (2,3,10,16). Other cardiovascular alterations have also been reported, including decreased cardiac function (21,25), decreased aerobic capacity (13), changes in vascular structure and function (10,29) and possible cardiac rhythm abnormalities (6,9).

Head-down tilt bed rest has become a primary research tool to examine mechanisms and test countermeasures for cardiovascular alterations. There is abundant literature supporting the utility of bed rest as an analog for multiple organ systems. One of the drawbacks of bed rest literature is the lack of standardization. This study is part of a NASA Flight Analogs Project initiative to conduct multisystem research on bed rest subjects under strictly standardized conditions.

We tested the hypothesis that arterial flow-mediated dilation responses, dilation in response to nitroglycerin and arterial structure would all change during bed
rest. Additionally, we tested the hypothesis that arteries in the arm would follow different patterns of change than arteries in the leg during head-down tilt bed rest. No bed rest study to date has addressed this possibility. Finally, we tested the hypothesis that orthostatic tolerance would decrease following bed rest.

Spaceflight and bed rest may also induce changes in cardiac function. Recent work has shown a decrease in ventricular mass (21,24) and stroke volume (5,15,21); however, more comprehensive measures of cardiac function are lacking. In addition to the above standard measures, we studied the effects of bed rest on numerous other indicators of cardiac function such as isovolumic relaxation time and myocardial performance index. We tested the hypothesis that cardiac function, as measured by echocardiography, would be decreased by exposure to bed rest.

METHODS

General

Refer to Meck, et al. (17) for description of the protocol, general conditions of the study and the use of long duration head-down tilt bed rest as a model for spaceflight. Bed rest and test protocols were reviewed and approved by the Johnson Space Center Committee for the Protection of Human Subjects, the University of Texas Medical Branch (UTMB) Institutional Review Board and the UTMB General Clinical Research Center Science Advisory Committee. Subjects
received verbal and written explanations of the bed rest and test protocols prior
to providing written informed consent.

Subjects
Data from 13 subjects are included in this study (eight men and five women).
Three subjects experienced 60 days of head-down tilt bed rest, six subjects
experienced 90 days of head-down tilt bed rest and four subjects experienced
44-53 days of head-down tilt bed rest (truncated due to Hurricane Rita, no post-
bed rest data were acquired on these subjects). Testing on females was timed to
always occur during the first six days of the menstrual cycle in order to minimize
the effects of estrogen and progesterone on the cardiovascular system.

Plasma Volume
Plasma volume was measured by the carbon monoxide rebreathing (CORB)
technique as previously reported (14,26). In this study, plasma volume was
corrected (plasma volume index, PVI) by body surface area (BSA).

$$BSA(m^2) = 0.007184 \times (Weight(kg)^{0.425}) \times (Height(cm)^{0.725})$$

Flow-Mediated Dilation
Subjects were placed in the supine position and instrumented with a three-lead
ECG. A Dinamap automatic blood pressure cuff (Johnson & Johnson, Arlington,
TX) was placed on the non-imaged arm to obtain a baseline blood pressure. An
occlusive pressure cuff (D. E. Hokanson, Inc., Bellevue, WA) was applied to the
limb used for imaging. Imaging of the brachial artery was performed by a registered sonographer using a Philips HDI 5000 (Bothel, WA) with a 12 MHz transducer above the antecubital fossa. When the optimal imaging site was acquired, the site was marked with a permanent marker and the same position was used throughout the study. In addition, ultrasound images from the initial procedure were printed and reviewed prior to subsequent imaging sessions. When possible, arterial branches were included as landmarks. Furthermore, a photograph was taken during the procedure to show the position of the transducer on the skin. This photograph was used to ensure proper placement of the ultrasound probe for subsequent tests.

Resting diameter images of the brachial artery in the arm were optimized to allow clear visualization of the intimal-medial borders. The images were then enlarged to improve the accuracy of subsequent measurements. Three images at end-diastole and three at peak systole were stored digitally for off-line analyses. Blood flow parameters including peak systolic velocity, pulsatility index and velocity time interval were also evaluated and stored. After acquisition of baseline images, an occlusive cuff (Hokanson) was inflated to 50 mmHg above the resting systolic pressure and cessation of flow was verified by Doppler ultrasound. The cuff remained inflated for five minutes, at which point the cuff was rapidly deflated. Pulsed Doppler of the flow response was stored at 10 and 20 seconds post-deflation. Images of the brachial artery were stored every 15
seconds, starting at 30 seconds post-deflation and continued until the third minute. Additional images were acquired at minutes four and five.

Flow-mediated dilation of the anterior tibial artery in the leg was accomplished following a similar protocol. The anterior tibial artery was chosen because it is of similar size to the brachial artery and is superficial enough to obtain high quality ultrasound images. The occlusive cuff was placed just proximal to the knee and was inflated to 70 mmHg over resting systolic blood pressure. This pressure was maintained for seven minutes on the leg prior to deflation. The remainder of the procedure was identical to that used for the brachial artery, described above. Preliminary results in our lab have shown that this protocol achieved a similar hyperemic response to that seen in the arm at 50 mmHg supra-systolic pressure for five minutes (data not shown).

Measurement and analysis of data were performed off-line on a desktop computer using ProSolv Cardiovascular Analyzer 3.0.50 (Indianapolis, IN). Measurements were made during diastole for consistency. Each image was measured by two experienced sonographers in a double-blind fashion. If a significant (greater than 10%) discrepancy between the two analyses was found, a third sonographer repeated the measurement. Doppler measurements and calculations were performed by an automated analysis feature of the ultrasound system.
For intimal-medial thickness measurements, three diastolic brachial artery images were stored at the R wave and three systolic images were stored at the end of the T wave from a superimposed ECG. The still frame images were stored in DICOM format and analyzed off line on Prosolv Cardiovascular Analyzer 3.0.50 (Indianapolis, IN). The posterior segment of the artery was enhanced with a Region Of Interest (ROI) magnification tool. Intimal-medial thickness measurements were made by two independent and blinded sonographers from three sequential images taken at the R wave. The measurements were made, with a caliper tool, from the central region of each image. The anterior interface of the intima was selected as the first linear interface echo; the second caliper was set at the medial adventitia line, defined as the next linear interface followed by a dark separating line.

Direct Arterial Dilation

Imaging of the brachial and anterior tibial arteries after administration of nitroglycerin (0.4 mg sublingual) was performed on the same day as, but no sooner than one hour after the completion of, the flow-mediated dilation procedure. The same imaging techniques and imaging locations were used as previously described.

Three baseline images were acquired and digitally stored at end-diastole prior to administration of sublingual nitroglycerin. The artery was imaged continuously throughout the session to assure the same position was maintained. Starting at
three minutes after the nitroglycerin administration, three images per minute were stored digitally for off-line analysis. One image per minute was measured live to monitor the time course of dilation. Imaging was continued until two minutes following the peak dilator response. The images were analyzed off-line by experienced sonographers who were blinded to the subject information. Any discrepancies greater than 10% were re-evaluated by a third sonographer.

Cardiac Function

Subjects were placed in the left lateral decubitus position. During head-down tilt bed rest, the subjects maintained the 6° head-down tilt. American Society of Echocardiography standards were used in acquiring images (HDI 5000, Philips Medical, Bothel, WA). M-mode echocardiography was used to measure interventricular septal thickness (IVST), posterior wall thickness (PWT) and left ventricular diameter in systole (LVEDS) and diastole (LVEDD). From these measurements, calculations of systolic function were made, including ejection fraction, stroke volume, velocity of circumferential shortening and left ventricular mass. Left ventricular mass was calculated as follows: 

\[ LVM \text{ (g)} = 0.8 \times 1.05 \times \left[ \left( LVEDD + IVST + PWT \right)^3 - \left( LVEDD \right)^3 \right] + 0.6 \] 

Myocardial performance index (MPI), a global measure of both systolic and diastolic function, was calculated as the ratio of left ventricular isovolumic contraction time plus isovolumic relaxation time divided by ejection time. Assessment of all the valves was accomplished using pulsed, continuous and color Doppler. Images were stored digitally and on videotape for subsequent off-line analysis. The echocardiography protocol
utilized views consistent with standards established by the American Society of Echocardiography (ASE).

**Tilt Test**

Subjects were placed on a tilt table and a Dinamap blood pressure cuff was placed on the upper arm. A Finapres (Ohmeda Medical, Netherlands) finger blood pressure cuff was placed on a finger of the opposite hand for continuous blood pressure measurement. Continuous measures of heart rate, ECG, arterial pressure and aortic blood flow [systolic velocity integral obtained by Doppler ultrasound (2 MHz probe) of the proximal ascending aorta] were recorded for five minutes while supine (pre-bed rest) or at 6° head-down tilt (BR44-BR60), and during tilt. This technique has been validated by previous studies (19,23). Beat to beat stroke volume (systolic velocity integral X cross-sectional area) determined by two-dimensional ultrasound (2–4 MHz phased array probe) at cusp insertion, cardiac output (stroke volume X heart rate) and total peripheral resistance (mean arterial pressure/cardiac output) were all calculated off-line. The subjects were then tilted upright to 80º for 30 minutes or until symptoms of presyncope intervened.

**Data and Statistical Analysis**

All vascular measurements and plasma volumes were taken as close as possible to BR-5 (baseline) and at days BR7, BR21, BR35, BR49, BR60, BR90 and at BR+3 post-bed rest. Statistical analysis was only performed for the first 60 days
of the study due to the low number of subjects that completed the entire 90 day protocol.

Data are presented as mean ± standard error unless otherwise noted. Statistics were performed on a desktop computer using SigmaStat® commercial software v. 3.1 (Richmond, CA). All data were tested for normality (Kolmogorov-Smirnov test) and equal variance (Levene Median test). Plasma volume, cardiac parameters and vital statistics were analyzed using a 1-way Repeated Measures ANOVA with a Bonferroni corrected pairwise comparison. Intimal-medial thickness was compared with a 2-way ANOVA with a Bonferroni correction for pairwise comparisons. Flow-mediated dilation and nitroglycerin data failed the normality test and were compared using Friedman's Repeated Measures ANOVA on ranks. Pairwise comparisons were made using Tukey’s test. Tilt data were analyzed with a Kaplan-Meier survival analysis comparing pre-bed rest data with data from BR44-BR60. Significance for all tests was accepted at \( P \leq 0.05 \).

RESULTS

Vital statistics and baseline hemodynamic measurements are shown in Table I. No differences were found during bed rest for systolic or diastolic blood pressure, heart rate, weight or body mass index.

Plasma Volumes
Plasma volumes index (PVI, plasma volume / body surface area), is shown in Figure 1 for baseline through 90 days of bed rest. Baseline PVI was 1.49 ± 0.126 L/m\(^2\). By day BR7, PVI fell significantly by 15%, to 1.26 ± 0.166 L/m\(^2\) (\(P < 0.001\)). By day BR49 of bed rest, PVI was 1.22 ± 0.095 L/m\(^2\) (\(P < 0.001\)), a total decrease of 18%. There were no differences between days BR7, BR21, BR35 or BR49 of bed rest (\(P = NS\)).

Arterial Function

Flow-Mediated Dilation

Flow-mediated arterial dilations (Figure 2) are expressed, on the y-axis, as the difference between the percent dilation on the bed rest day minus the percent dilation during the pre-bed rest baseline (delta). The responses of the brachial artery did not change (\(P = NS\)); however, dilation was significantly increased in the anterior tibial artery by BR49 (day effect, \(P = 0.001\)).

Direct Arterial Dilation

There were no differences between bed rest days for dilations induced by the nitric oxide (NO) donor nitroglycerin (Figure 3, \(P = NS\) in the brachial or the anterior tibial artery). However, there was a significant difference in the dilator response between the brachial artery and anterior tibial artery (treatment effect, \(P < 0.001\)).

Intimal-Medial Thickness
The thickness of the arterial wall, shown in Figure 4, decreased significantly during bed rest for the anterior tibial artery \( (P < 0.001) \), but not in the brachial artery, when compared to the baseline value. This effect was seen at days BR21, BR35 and BR49. There was also a significant difference between the brachial and anterior tibial artery (treatment effect, \( P = 0.001 \)).

**Cardiac Function**

Measures of cardiac function are shown in Table II. Significant decreases during bed rest were seen in left ventricular systolic diameter (BR7, \( P = 0.035 \); BR49, \( P = 0.005 \)), left ventricular diastolic diameter (\( P = 0.015 \) at BR21), IVRT (\( P < 0.025 \) for days BR7, BR21, BR31 and BR49) and ejection time (\( P < 0.03 \) on days BR21, BR31 and BR49). Myocardial performance index increased, which indicates a decrease in performance, and became statistically significant by day BR7 (\( P < 0.033 \)) and was also significantly higher at days BR31 and BR49 (\( P < 0.005 \)).

**Tilt Test**

The ability of test subjects to tolerate 80° upright tilt was analyzed with a Kaplan-Meier survival analysis (Figure 5). There was a trend (\( P = 0.1 \)) for survival to be lower following 60 days of bed rest when compared to pre-bed rest results.

**DISCUSSION**

Resources on the remaining Space Shuttle flights and the International Space Station are extremely limited. It is clear that ground based analogs to spaceflight
will be critical to expand our understanding of the causes of spaceflight induced decrements in cardiovascular function. Head-down tilt bed rest has been used as a model for spaceflight, however the lack of standardization and varying durations of bed rest complicate interpretation. Our data show that cardiovascular alterations during longer term, head-down tilt bed rest are similar to those seen in spaceflight.

Plasma Volume

The time course and magnitude of plasma volume loss is critical to the understanding of the mechanisms linking bed rest and spaceflight. While plasma volume is not the separating factor in determining presyncope in crewmembers (16,27), it is believed to be the triggering mechanism that leads to subsequent dysfunction. Previous bed rest reports detail plasma volume losses ranging from 4% to 17%, depending on the protocol (26), which is similar to the data presented here. Our data are also similar to those reported from spaceflight (16,26) which show plasma volume losses ranging from 7% to 19.5%. These new data show that the entire plasma volume loss occurs within the first seven days (our earliest time point), and is maintained in a steady state throughout the 49 days of bed rest (Figure 1). The fluid balance data shown in the overview section of this issue (17) shows an early, marked diuresis which confirms the plasma volume data. These results are consistent with spaceflight data as well. It has been shown that plasma volume is reduced by 16% by day 2 of spaceflight and 11% at day 7-8 of spaceflight (12). In these bed rest subjects, there was a trend for decreased orthostatic tolerance and three of these ten (30%) were
unable to complete ten minutes of tilt (Figure 5). This is nearly identical to the percentage of crewmembers unable to complete ten minutes of tilt following short duration spaceflight (27). Taken together, these data show that bed rest is a good model for spaceflight-induced plasma volume losses in both magnitude and time course.

**Arterial Function**

This study used a new approach to study arteries by measuring both structure and function. In addition, we compared and contrasted responses from an artery in the arm (brachial) and a similar sized artery in the leg (anterior tibial) during bed rest. This approach has added important new information. In the brachial artery, none of the measured responses changed over the course of bed rest. Conversely, in the anterior tibial artery there were two important changes. First, the intimal-medial thickness was profoundly reduced. This confirms findings in animal studies and suggests that the vascular smooth muscle itself remolds in response to disuse during bed rest. Prior work from this laboratory suggests that the fluid shifts and relative hypovolemia, precipitated by both bed rest and spaceflight, may cause a loss of interstitial fluid volume (24), which could cause a change in function independent of contractile dysfunction. In cardiac tissue, dehydration causes diastolic dysfunction due to ventricular stiffening (25). In smooth muscle it could also increase stiffness. In addition, dehydration could reduce the diffusion distance from the endothelial layer, so that a greater concentration of NO reaches the smooth muscle.
Not all vascular beds respond to simulated microgravity in a parallel fashion. There are recent reports from several groups detailing structural remodeling of resistance vasculature in rats after hind limb suspension (8,22,29). In this model, the rat is suspended by the tail to achieve fluid shifts similar to those in microgravity. As a result, the forelimbs are utilized for locomotion more than during control, and the hind limbs are utilized less. This causes changes in the two primary mechanical forces that act on the vasculature: transmural pressures and shear stress. During suspension, these forces increase in the forelimbs, but decrease in the hind limbs. Both the smooth muscle and the endothelium respond to these changes. Vasculature in the forelimbs show hypertrophic remodeling while that in the hind limbs show atrophic remodeling (28). Following hind limb suspension, vasodilatory responses to acetylcholine injections (an endothelium-dependent response) are reduced in the femoral artery and soleus arterioles (22), both of which have been exposed to reduced blood flow and shear stress, but increased in the carotid artery, which has been exposed to increased blood flow and shear stress (11). The media cross-sectional area in arteries also decreases in the hind limb (8,22), but not the forelimb, suggesting atrophic remodeling in the hind limb (8). The hind limb vessels also have a diminished responsiveness to vasoconstrictors (7).

The second change in anterior tibial artery function over the course of bed rest was an increase in flow-mediated dilation. This could be related to the change in
wall thickness discussed above, as a thinner arterial wall may allow a greater concentration of NO to reach the smooth muscle cells. The third response, dilation in response to sublingual nitroglycerin, was unchanged. At first glance, these findings may seem incongruent; however, they can be reasonably explained. Flow-mediated dilation and sublingual nitroglycerin provide the vascular smooth muscle cells with the dilator nitric oxide by two very different mechanisms. The first provides NO indirectly but locally via the endothelium. The second provides NO directly but systemically. Our results show that a defect in the signal transduction cascades in the smooth muscle is unlikely, as there is no systemic change in endothelium-independent NO dilation.

In animal studies, arterial function is usually tested with local intra-arterial injections of vasoactive substances or ex-vivo preparations. Unfortunately, our institutional constraints do not allow intra-arterial injections in bed rest subjects. Thus, we measured arterial function only from the standpoint of changes in the dilatory function of the arteries. Rat data suggests arterial smooth muscle in the lower body would be less able to constrict following head-down tilt (29). We are currently assessing arterial constrictor function in a hypovolemia model which has produced changes in left ventricular (LV) mass similar to spaceflight.

**Cardiac Function**

This is the most complete echocardiographic assessment of resting cardiac structure and function during long duration bed rest of which we are aware. We
found several measures that indicated a decrement in cardiac structure and in both systolic and diastolic function.

Left ventricular mass did not change during this study. Conversely, LV mass has been reported to be decreased after spaceflight by both MRI (21) and ultrasound techniques (24). We have previously shown, through mathematical modeling, that the post-spaceflight decrease in LV mass is most likely due to interstitial dehydration of the myocardium secondary to spaceflight-induced hypovolemia (24). Unfortunately, LV mass has never been measured during spaceflight so it is not known if the same effect would occur in the absence of gravity. In the current study, LV mass was measured during head-down tilt, but not measured after the subjects resumed ambulatory activity. This may explain the absence of change in LV mass. A suggestion for future bed rest campaigns is to add a measurement early during post-bed rest reconditioning.

Despite the lack of change in LV mass, there were several changes in cardiac function. It is not clear which, if any of these, occurred in response to the decrease in preload caused by the hypovolemia. However, the degree of change suggests true changes in function. In Table II we show that some, but clearly not all measures of cardiac performance are changed following bed rest. There is no consensus as to which measures best represent clinically relevant dysfunction in bed rested subjects; however, some interesting trends can be gleaned from these data. Isovolumic relaxation time increased significantly during bed rest,
indicating decreased diastolic function. This is similar to results obtained following spaceflight (24). Myocardial performance index, a global measure of function which accounts for both systolic and diastolic parameters, showed a decrease in performance, suggesting an overall decrease in cardiac function. It is not unusual that echocardiographic measurements of cardiac function seem to contradict each other (4). Each measurement corresponds to parts of the heart which are subject to different degrees of influence by aortic, atrial and ventricular pressures and volumes. The heterogeneous nature of these results does not invalidate their usefulness, rather they illustrate that the effects of bed rest on cardiac function are complex and multifactorial. We have previously reported changes in cardiac function following long duration spaceflight that also show a heterogeneous pattern (15); however, that study lacked some of the more mechanistic measurements that we now present. From the data in this study, it appears as though bed rest and long duration spaceflight both alter cardiac function. It is not clear if these changes are the result of decreases in fluid volume and preload, or if they represent a true change in cardiac muscle function. Future spaceflight studies should include more detailed echocardiograms to allow for a more direct comparison.

One primary concern is that most measures of cardiac function are somewhat preload dependent. It is well known that preload changes during bed rest, similar to spaceflight, due to the pronounced fluid redistribution-induced decrease in plasma volume. This could explain the increase in MPI seen at BR7 and BR21
(Table II). However, it does not explain why MPI further increases on BR31 and BR49 because plasma volume has stabilized. It could be that plasma volume accounts for the initial response and another mechanism drives the changes seen following 35 days of bed rest. The second mechanism could include cardiac deconditioning due to the decreased aerobic activity required during bed rest. This could lead to a decrease in contractility or possibly a remodeling of the myocardium (as supported by decreases in LV diameters, but not LV mass).

While we were unable to perform statistical analysis on the time points beyond BR49, there are obvious trends that suggest that the cardiac changes persist to 90 days. Further examination of later time points will provide more insight into the ramifications of long term bed rest, and potentially longer term spaceflight, on the cardiovascular system.

Limitations

A major limitation of this study is the subject number at the varying time points. This is largely due to the forced evacuation of subjects for Hurricane Rita. Therefore, these subjects only completed 44-53 days of the designed 90 day bed rest protocol, and only a relatively small number of subjects completed 90 days of bed rest. We have chosen to limit our statistical analysis in this report to the first 60 days of bed rest (although we show all data in the figures) in order to utilize the data points shared by the most subjects.

ACKNOWLEDGEMENTS
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REFERENCES


Table I. Vital Statistics and Baseline Memodynamics.

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<th>pre-Bed rest</th>
<th>BR 7</th>
<th>BR 21</th>
<th>BR 35</th>
<th>BR 49</th>
<th>BR 60</th>
<th>BR 75</th>
<th>BR 90</th>
<th>BR+3</th>
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<tr>
<td><strong>Height, m</strong></td>
<td>1.7 ± 0.1</td>
<td></td>
<td></td>
<td></td>
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<td></td>
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<tr>
<td><strong>Weight, kg</strong></td>
<td>72.6 ± 16.6</td>
<td>72.0 ± 17.0</td>
<td>72.9 ± 14.3</td>
<td>71.4 ± 16.0</td>
<td>69.8 ± 16.1</td>
<td>65.8 ± 14.2</td>
<td>71.4 ± 24.2</td>
<td>62.9 ± 16.8</td>
<td>65.8 ± 15.2</td>
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<td><strong>Body Mass Index, kg/m²</strong></td>
<td>25.4 ± 4.2</td>
<td>24.6 ± 4.4</td>
<td>25.4 ± 3.7</td>
<td>24.7 ± 4.3</td>
<td>24.5 ± 4.1</td>
<td>23.6 ± 4.2</td>
<td>26.5 ± 5.9</td>
<td>23.4 ± 4.6</td>
<td>23.7 ± 4.5</td>
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<td><strong>Systolic Pressure, mmHg</strong></td>
<td>118.8 ± 13.2</td>
<td>116.1 ± 8.1</td>
<td>118.7 ± 16.2</td>
<td>115.9 ± 10.9</td>
<td>118.2 ± 13.4</td>
<td>116.7 ± 13.9</td>
<td>105.2 ± 8.2</td>
<td>112.7 ± 15.3</td>
<td>109.8 ± 12.0</td>
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<td><strong>Diastolic Pressure, mmHg</strong></td>
<td>67.8 ± 8.4</td>
<td>68.3 ± 7.2</td>
<td>69.4 ± 8.8</td>
<td>70.9 ± 6.7</td>
<td>70.5 ± 6.9</td>
<td>69.1 ± 8.3</td>
<td>69.3 ± 7.1</td>
<td>73.5 ± 12.8</td>
<td>68.2 ± 8.8</td>
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<td><strong>Heart Rate, beats/min</strong></td>
<td>65.3 ± 8.9</td>
<td>63.0 ± 10.3</td>
<td>65.5 ± 7.7</td>
<td>65.7 ± 11.0</td>
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<td>69.5 ± 13.1</td>
<td>67.8 ± 11.9</td>
<td>69.3 ± 13.6</td>
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Table II. Echocardiography Results for Systolic Function, Morphology and Diastolic Function During Pre-Bed Rest, Days BR7, BR21, BR31 and BR49 of Bed Rest. Statistical Analyses are Included in Separate Columns.

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<thead>
<tr>
<th>Parameter</th>
<th>Pre bed rest</th>
<th>Day 7</th>
<th>P value</th>
<th>Day 21</th>
<th>P value</th>
<th>Day 31</th>
<th>P value</th>
<th>Day 49</th>
<th>P value</th>
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<td>LV diastolic diameter (cm)</td>
<td>4.94</td>
<td>4.83</td>
<td>NS</td>
<td>4.68</td>
<td><strong>0.015</strong></td>
<td>4.79</td>
<td>NS</td>
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<td>LV systolic diameter (cm)</td>
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<td>2.78</td>
<td><strong>0.035</strong></td>
<td>2.84</td>
<td>NS</td>
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<td>NS</td>
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<td>Ejection fraction</td>
<td>69</td>
<td>73</td>
<td>NS</td>
<td>70</td>
<td>NS</td>
<td>70</td>
<td>NS</td>
<td>74</td>
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<td>LV mass (g)</td>
<td>118.7</td>
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<td>NS</td>
<td>119.2</td>
<td>NS</td>
<td>114.7</td>
<td>NS</td>
<td>109.9</td>
<td>NS</td>
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<td>Stroke volume</td>
<td>80.3</td>
<td>80.0</td>
<td>NS</td>
<td>71.6</td>
<td>NS</td>
<td>75.4</td>
<td>NS</td>
<td>77.6</td>
<td>NS</td>
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<td>Isovolumic relaxation time (msec)</td>
<td>72.9</td>
<td>85.0</td>
<td><strong>0.025</strong></td>
<td>83.9</td>
<td><strong>0.041</strong></td>
<td>95.9</td>
<td><strong>&lt;0.001</strong></td>
<td>89.2</td>
<td><strong>0.002</strong></td>
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<td>Isovolumic contraction time (msec)</td>
<td>49.1</td>
<td>53.3</td>
<td>NS</td>
<td>47.5</td>
<td>NS</td>
<td>53.0</td>
<td>NS</td>
<td>48.8</td>
<td>NS</td>
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<tr>
<td>Ejection time (msec)</td>
<td>299</td>
<td>287</td>
<td>NS</td>
<td>281</td>
<td><strong>0.028</strong></td>
<td>282</td>
<td><strong>0.041</strong></td>
<td>275</td>
<td><strong>0.002</strong></td>
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<tr>
<td>Myocardial performance index</td>
<td>0.41</td>
<td>0.49</td>
<td><strong>0.033</strong></td>
<td>0.47</td>
<td>0.082</td>
<td>0.53</td>
<td><strong>&lt;0.001</strong></td>
<td>0.51</td>
<td><strong>0.004</strong></td>
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</table>
CAPTIONS FOR FIGURES

Figure 1. Plasma volume changes during bed rest. Plasma volume index (PVI) is the plasma volume corrected by body surface area. Significant differences from pre-bed rest were seen at all timepoints. * indicates $P \leq 0.05$ within group for bed rest day.

Figure 2. Reactive hyperemic responses during bed rest. These graphs show the difference between pre- and post-occlusion (delta) for each timepoint. There were no statistical differences in the brachial artery (left panel) or in the anterior tibial artery (right panel).

Figure 3. Direct arterial dilation with nitroglycerin. These graphs show the difference between pre- and post-occlusion (delta) for each timepoint. There were no statistical differences in the brachial artery (left panel) or in the anterior tibial artery (right panel). There was a difference found between the brachial and anterior tibial artery. § indicates $P \leq 0.05$ between arteries.

Figure 4. Intimal medial thickness. The intimal medial thickness (cm) decreased during bed rest in the anterior tibial artery only (right panel). * indicates $P \leq 0.05$ within group for bed rest day compared to pre-bed rest.

Figure 5. Survival analysis of tilt test standing times. The solid line represents the probability of standing at each time point of the tilt test before bed rest. The dashed line represents the probability of standing following 44-60 days of bed rest. There is a trend for the survival to be lower at day 44-60 than during pre-bed rest ($P = 0.1$).
Figure 1.
Figure 2.

Brachial Artery

Anterior Tibial Artery
Figure 3.

Brachial Artery

Anterior Tibial Artery
Figure 4.
Figure 5.

Survival Probability

Time

Pre-bed rest
Bed rest day 60

n = 9, p = 0.1