

Carbon nanofiber nanoelectrodes for neural stimulation and chemical detection:  
The era of “smart” deep brain stimulation

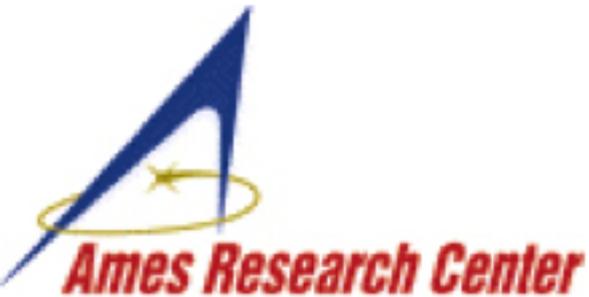
Jessica E. Koehne, NASA Ames Research Center, Moffett Field, CA

A sensor platform based on vertically aligned carbon nanofibers (CNFs) has been developed. Their inherent nanometer scale, high conductivity, wide potential window, good biocompatibility and well-defined surface chemistry make them ideal candidates as biosensor electrodes. Here, we report two studies using vertically aligned CNF nanoelectrodes for biomedical applications. CNF arrays are investigated as neural stimulation and neurotransmitter recording electrodes for application in deep brain stimulation (DBS). Polypyrrole coated CNF nanoelectrodes have shown great promise as stimulating electrodes due to their large surface area, low impedance, biocompatibility and capacity for highly localized stimulation. CNFs embedded in SiO<sub>2</sub> have been used as sensing electrodes for neurotransmitter detection. Our approach combines a multiplexed CNF electrode chip, developed at NASA Ames Research Center, with the Wireless Instantaneous Neurotransmitter Concentration Sensor (WINCS) system, developed at the Mayo Clinic. Preliminary results indicate that the CNF nanoelectrode arrays are easily integrated with WINCS for neurotransmitter detection in a multiplexed array format. In the future, combining CNF based stimulating and recording electrodes with WINCS may lay the foundation for an implantable “smart” therapeutic system that utilizes neurochemical feedback control while likely resulting in increased DBS application in various neuropsychiatric disorders. In total, our goal is to take advantage of the nanostructure of CNF arrays for biosensing studies requiring ultrahigh sensitivity, high-degree of miniaturization, and selective biofunctionalization.

### Biography

Dr. Jessica E. Koehne is a research scientist at the NASA Ames Center for Nanotechnology where she leads the Nano-Biosensors Group. Her research interests include the interface between nanoscale materials, electronics and biological systems with an emphasis on biosensing. Dr. Koehne has developed carbon nanotube and nanofiber based sensor platforms for the detection of DNA, rRNA, proteins and neurotransmitters with applications ranging from point-of-care to homeland security. Dr. Koehne has published over 40 peer reviewed articles in the field of nanotechnology and has received numerous awards for technical achievement including the 2011 Presidential Early Career Award for Scientists and Engineers.





# **Carbon nanofiber nanoelectrodes for neural stimulation and chemical detection The era of “smart” deep brain stimulation**

**Jessica E. Koehne  
NASA Ames Research Center  
Moffett Field, CA**

# Outline

- Biosensing motivation
- Structure and fabrication of carbon nanofibers
- Application of carbon nanofiber electrodes in deep brain stimulation therapy
- Neurochemical recording by carbon nanofiber electrodes and Wireless Instantaneous Neurotransmitter Concentrator Sensor system

# NASA Ames Research Center

- Established in 1939 as the second laboratory of the National Advisory Committee for Aeronautics (named after NACA chair, Joseph S. Ames)
- Ames is 1 of 10 NASA field centers
- Located in the heart of the silicon valley
  - High-tech companies, start-ups, biotechnology
- Some of Ames Technical Areas
  - Astrobiology
  - Thermal protective systems
  - Simulation technology
  - Atmospheric science
  - Fundamental space biology
  - Human factors research
  - Nanotechnology



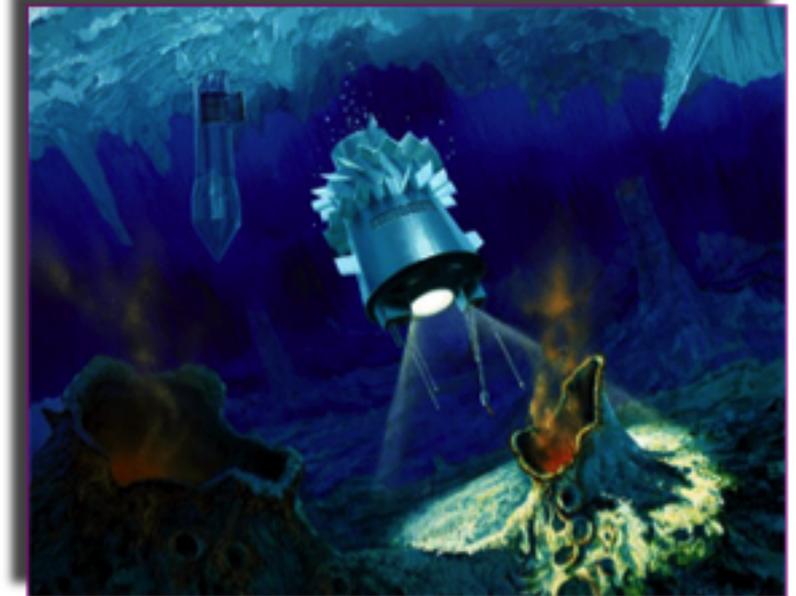


## NASA Applications

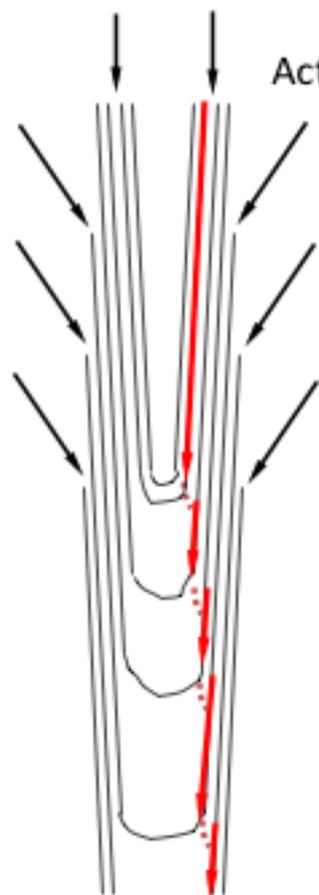
- Astronaut health monitoring
  - Lab-on-a-chip
- Water Quality monitoring
  - Pathogen detection on ISS and long duration missions
- Planetary exploration
  - Life on other planets

## Outside Applications and Customers

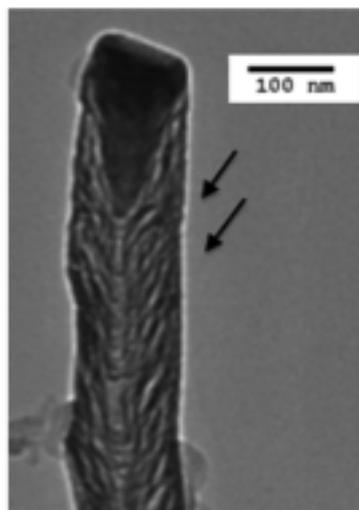
- Medical Diagnostics
  - NIH, DARPA
- Environmental Monitoring
  - EPA, NIH
- Biowarfare agent detection
  - DHS, DARPA
- Food Safety
  - FDA



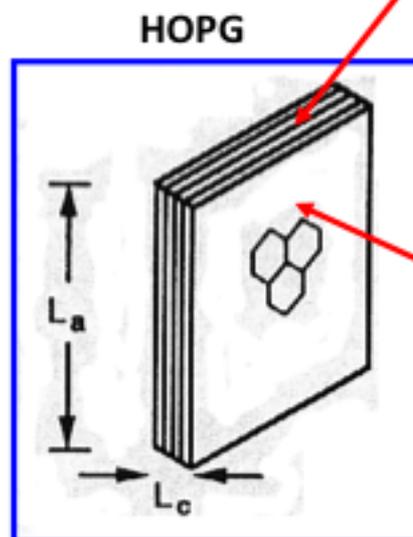
# What are Carbon Nanofibers (CNFs)?



Bamboo-like CNFs



TEM of CNF



R. L. McCreery, A. J. Bard, in *Electroanalytical Chemistry*, Ed., 1991, 17, 221.

## Edge Plane:

- (1) High electron transfer rate ( $\sim 0.1$  cm/s)
- (2) Very high specific capacitance ( $>60$   $\mu\text{F}/\text{cm}^2$ )

## Basal Plane:

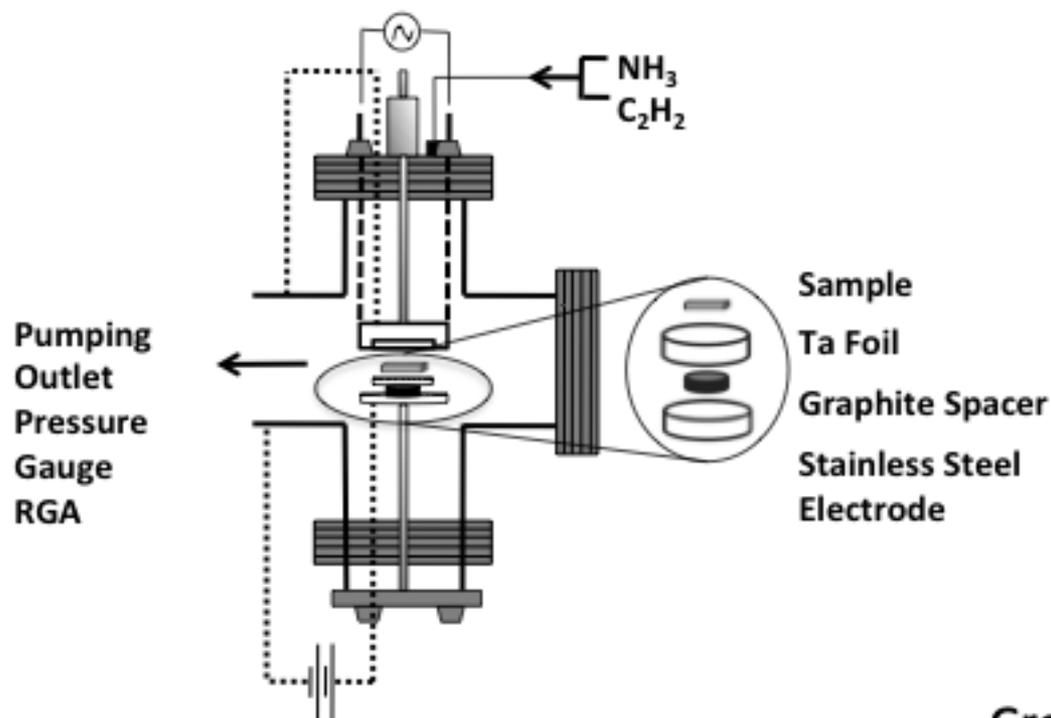
- (1) Low electron transfer rate ( $< 10^{-7}$  cm/s)
- (2) Anomalously low capacitance ( $\sim 1.9$   $\mu\text{F}/\text{cm}^2$ )

## Why CNF as biosensor electrode material?

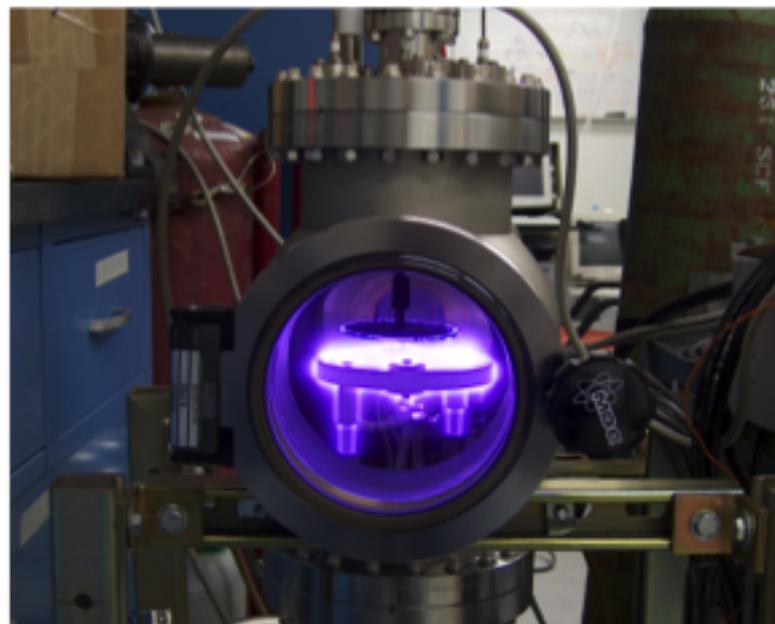
- 1) Good conductivity
- 2) Wide potential window
- 3) Many active sites for electron transfer
- 4) Easy to pattern, grow and process on silicon devices

# CNF Growth by Plasma Enhanced Chemical Vapor Deposition (PECVD)

PECVD Reactor Schematic



Custom Built PECVD Reactor

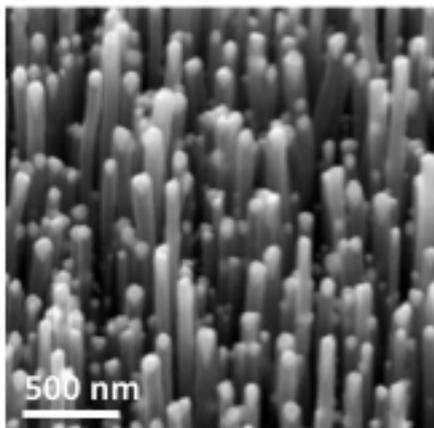


## Growth Process

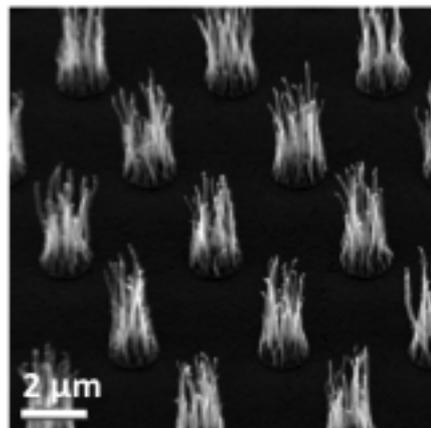
- Heated to 650 C
- Plasma discharge 500 W, 530 V, 0.97 A
- 150 sccm  $\text{NH}_3$ /50 sccm  $\text{C}_2\text{H}_2$ , 5-6 torr
- Growth rate- 1000 nm/min
- Quality is good, alignment is good

# Define CNF Placement by Catalyst Placement

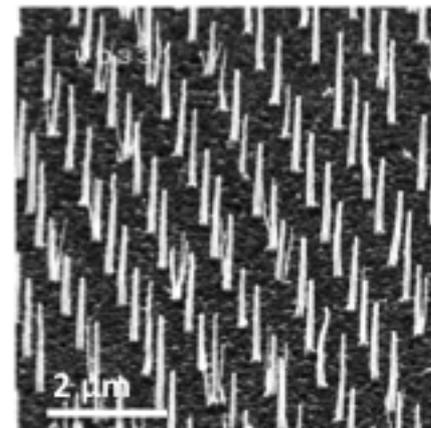
Continuous Layer of Catalyst



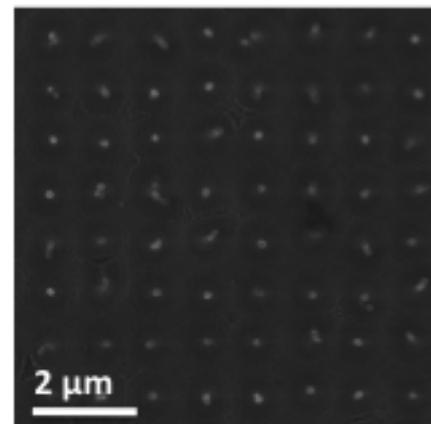
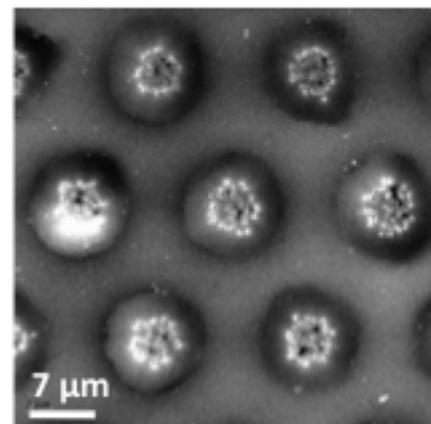
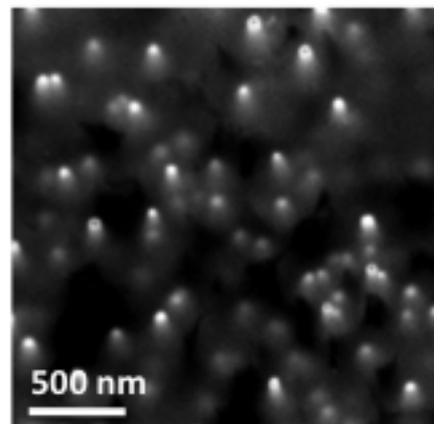
Photolithography Defined Catalyst Spots



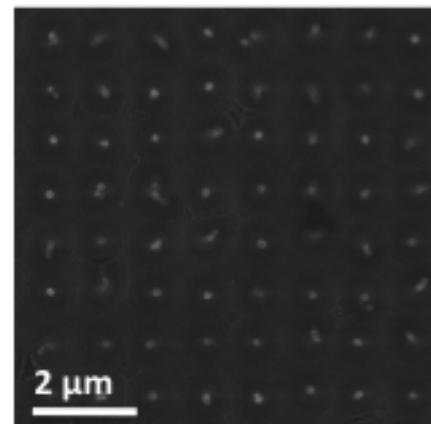
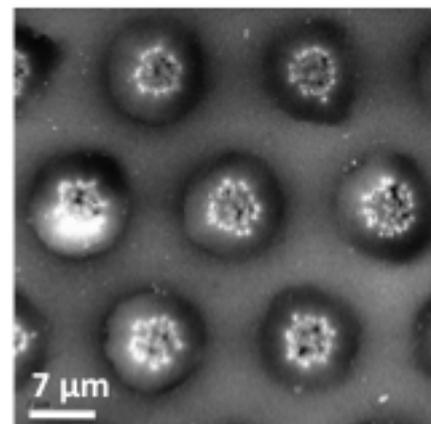
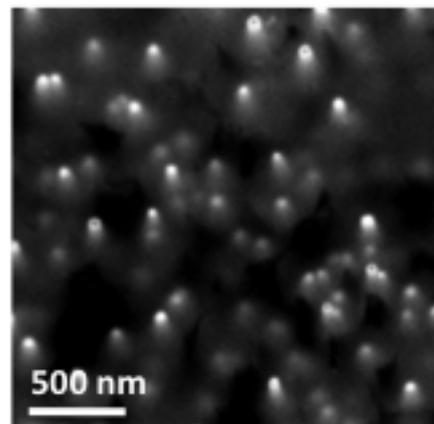
Electron Beam Lithography Defined Catalyst Spots



As Grown CNFs

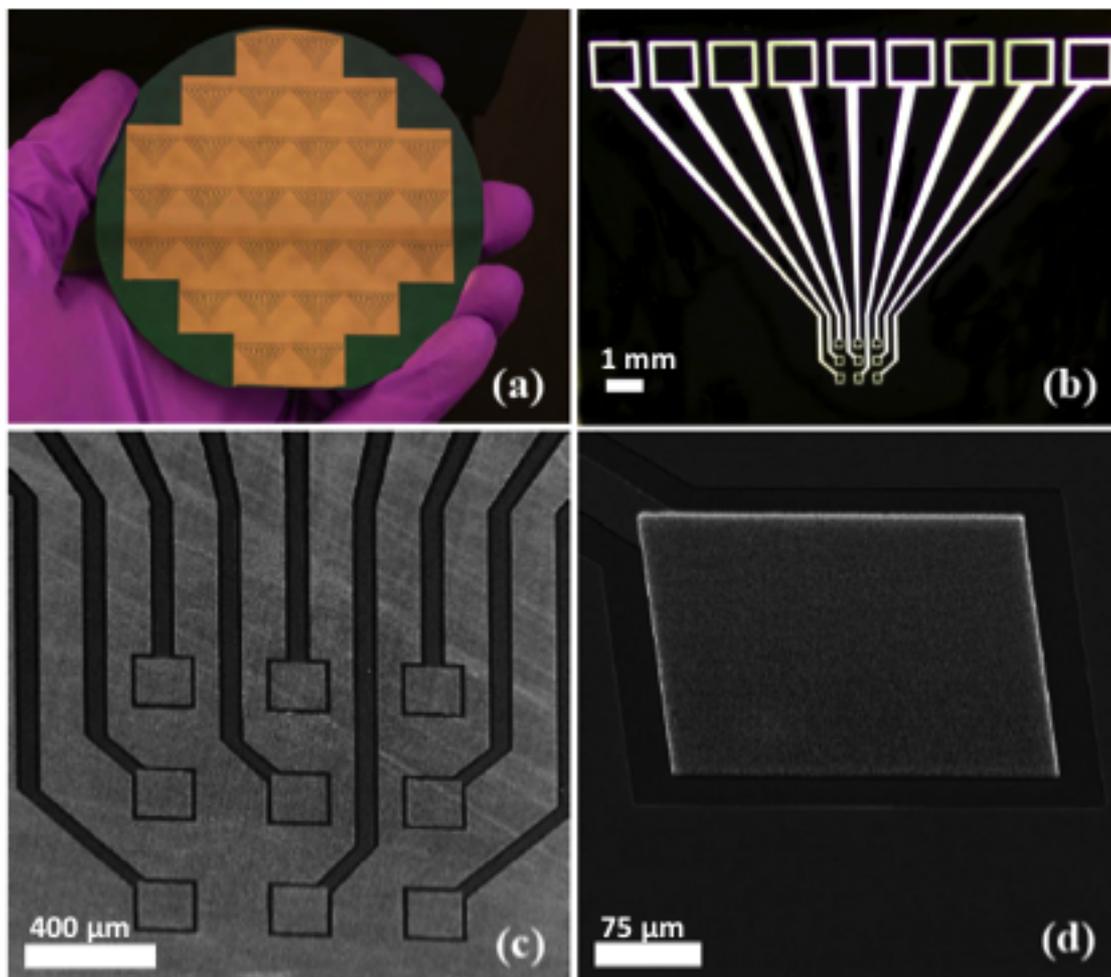


SiO<sub>2</sub> Encapsulated CNFs



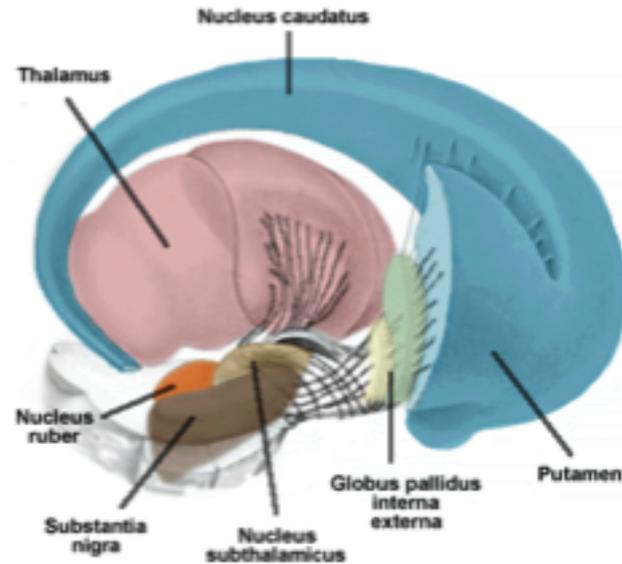
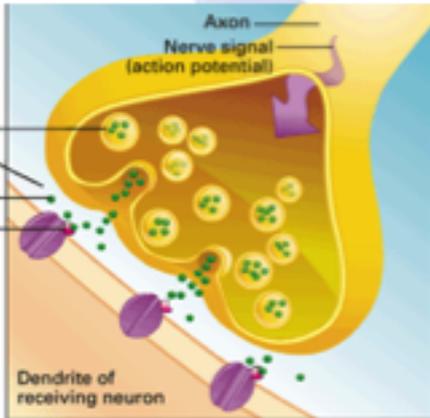
# Fabrication of 3x3 Array

30 devices on  
a 4" Si wafer



- 200  $\mu\text{m}$  by 200  $\mu\text{m}$  electrode dimensions
- 9 individually addressed electrodes
- potentially 9 different target molecules

# Motivation: Parkinson's Disease



Parkinson's disease is a neurodegenerative disorder in which patients have insufficient production of dopamine from dopaminergic cells in the substantia nigra

Current treatments include L-dopa, dopamine agonists, MAO-B inhibitors, surgery (ablation and deep brain stimulation)

# Deep Brain Stimulation



## Deep Brain Stimulation (DBS)

- Started in the 1960's
- Over 80,000 successful surgeries
- Has been demonstrated to be an effective neurosurgical treatment for several pathologies including:

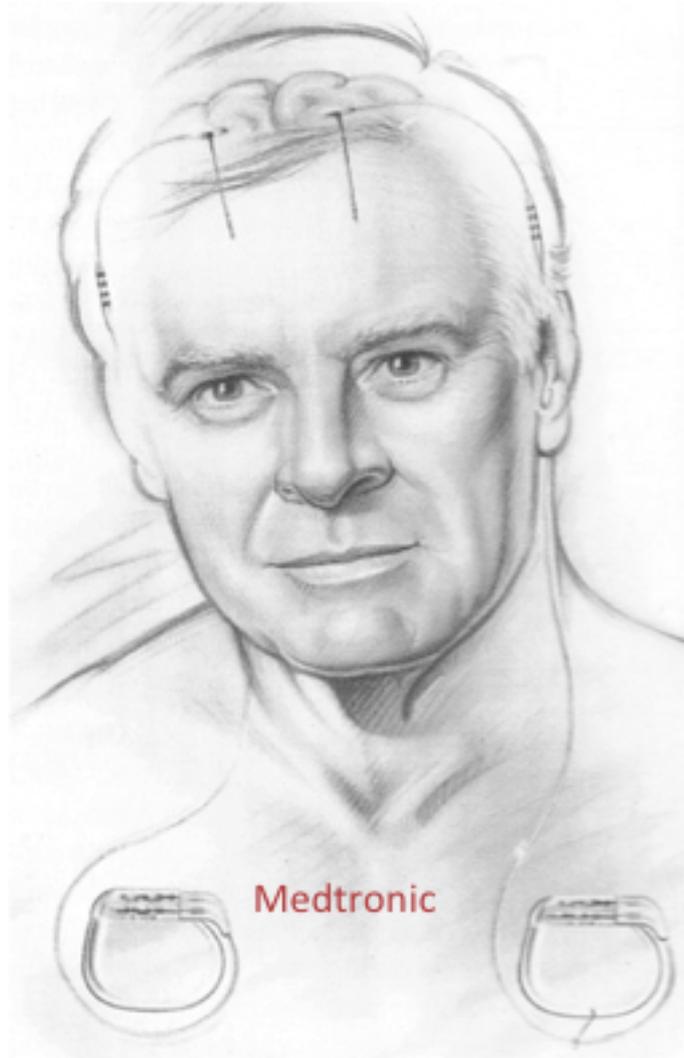
- tremor
- epilepsy
- Parkinson's disease
- depression
- Tourette syndrome
- chronic pain

## How DBS Works

- Brain pacemaker, electrical impulses to different areas of the brain
- Stimulation 24/7

## Potential Improvements

- Time consuming and difficult to program without feedback
- Want real-time monitoring of the neurochemical output
- Development of chemically-guided placement of DBS electrodes *in vivo*.



**Clinical efficacy is not questioned, but mechanisms are very poorly understood**

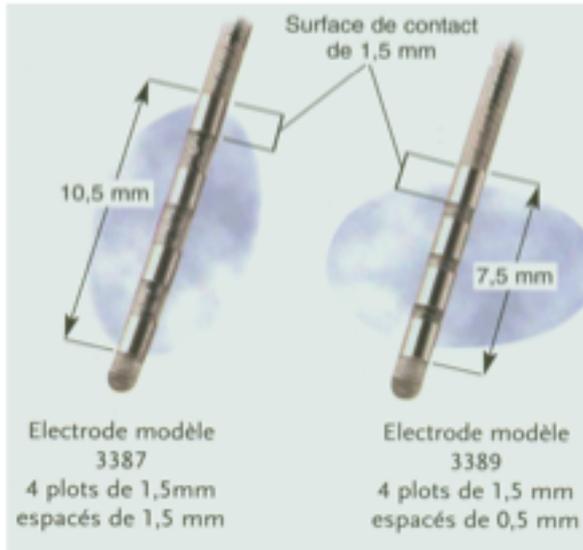


# History of DBS

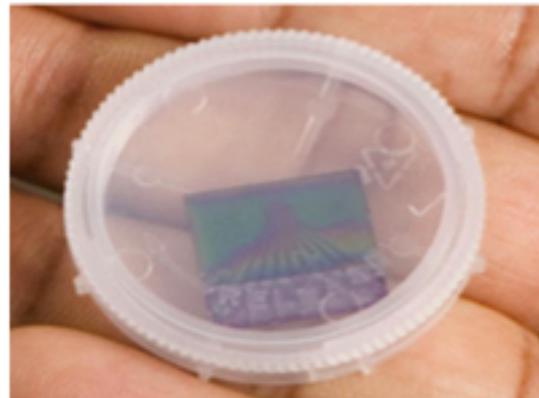
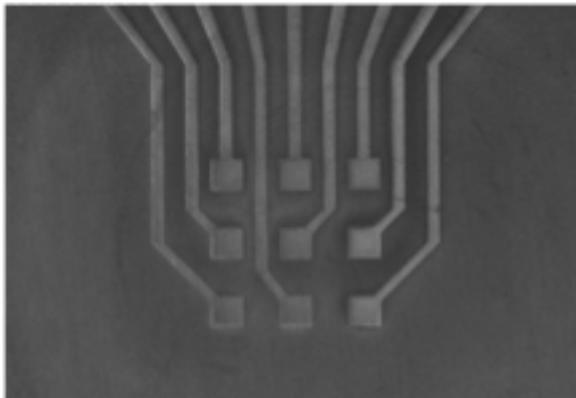


- DBS used for pain control since 1960s
- DBS for tremor began in Europe (1987)
- Europe: CE mark approval for
  - Activa<sup>®</sup> Tremor Control Therapy in 1993
  - Activa<sup>®</sup> Parkinson's Control Therapy in 1998
- USA: FDA approval for
  - Activa<sup>®</sup> Tremor Control Therapy in 1997
  - Activa<sup>®</sup> Parkinson's Control Therapy in 2002

## DBS Electrodes from Medtronic



## CNF Electrodes

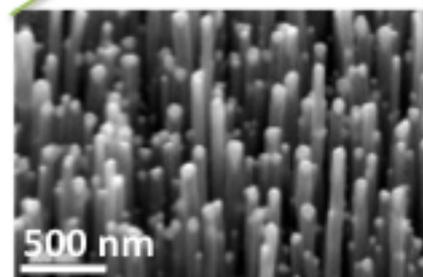
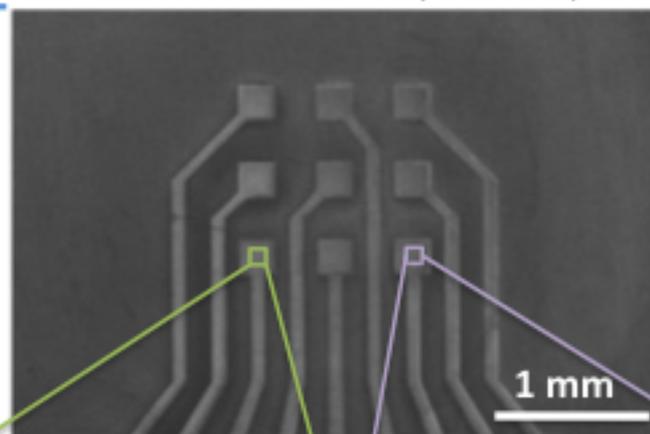


Current 3x3 CNF device does not have an optimal geometry for implantation but can be used to preliminary in vitro investigations.

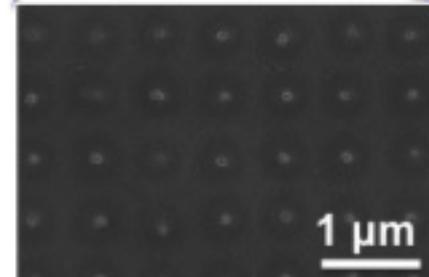
# CNF Array for Applications in Deep Brain Stimulation



Active Electrode Array at the Tip



**Stimulating Electrode:**  
Bare CNFs with high capacitance and low impedance



**Recording Electrode:**  
CNFs embedded in SiO<sub>2</sub> with ultrahigh sensitivity

## Goal:

Create a “smart” device based on a multiplexed CNF array for localized and efficient stimulation and neurochemical recording

**High Capacitance** ( $C_0 = \Delta i / 2v$ )

Noble metal  $\sim 20 \mu\text{F}/\text{cm}^2$

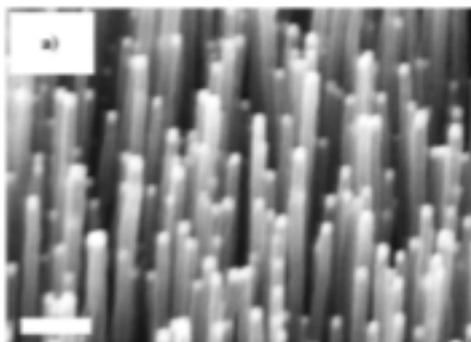
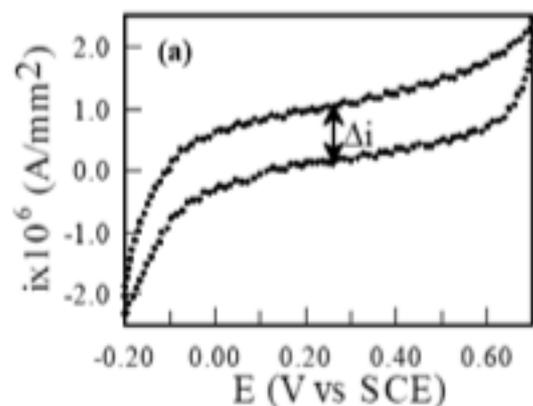
As-grown CNF array:  $0.4 \text{ mF}/\text{cm}^2$

Ppy-coated CNF array: 40 to  $100 \text{ mF}/\text{cm}^2$

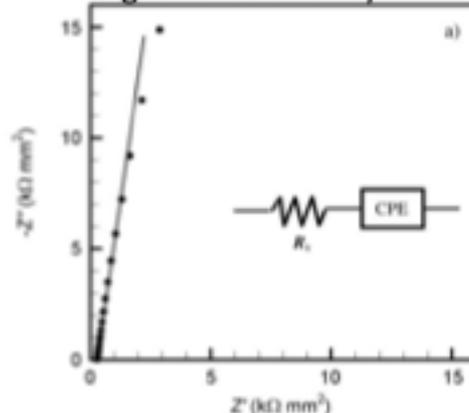
**Low Impedance**

At 1 kHz, the impedance is negligible compared to the solution resistance

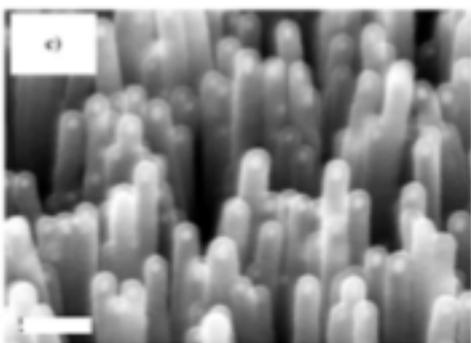
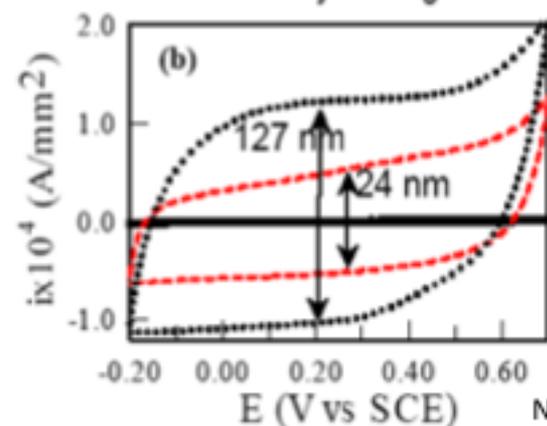
As-grown CNF Array



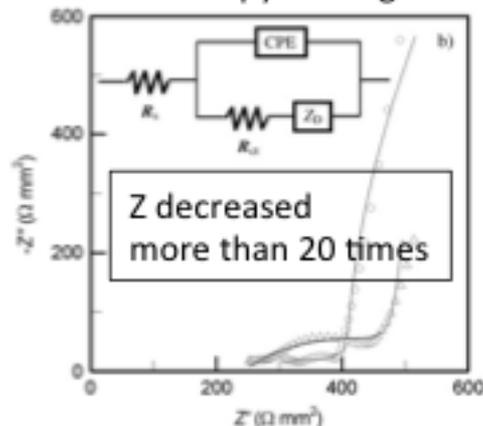
As-grown CNF Array



After PPy coating

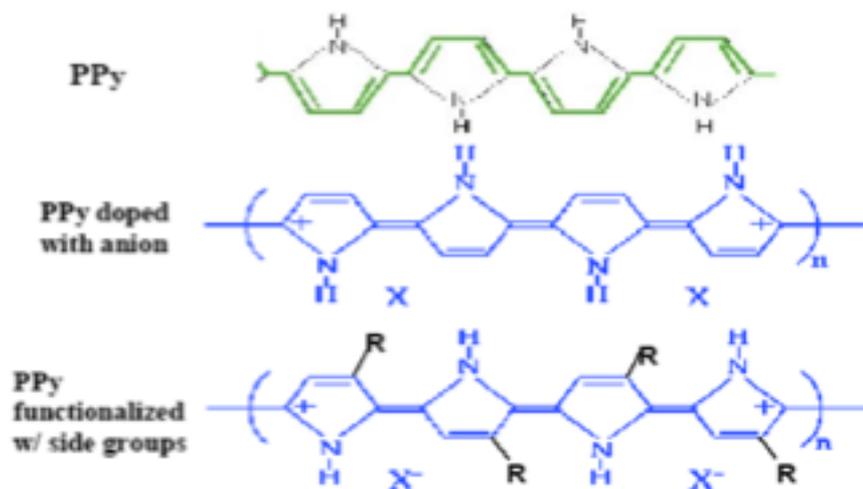


After Ppy coating



# Biocompatibility

## Optimization through chemical modification

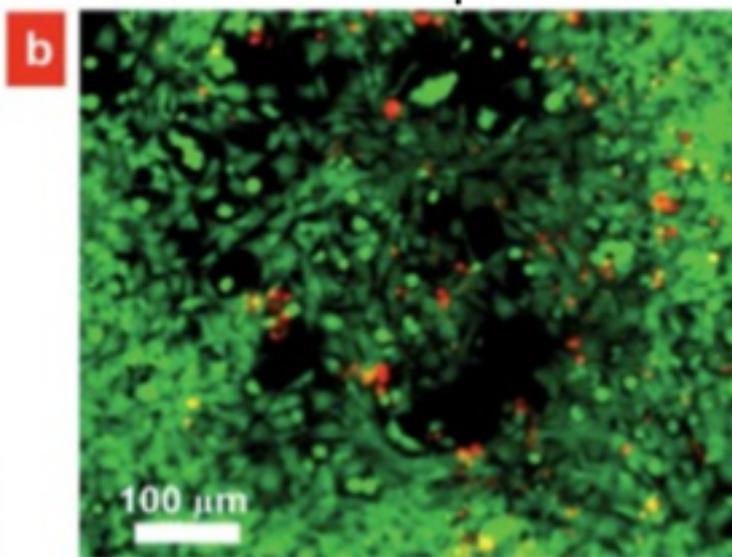
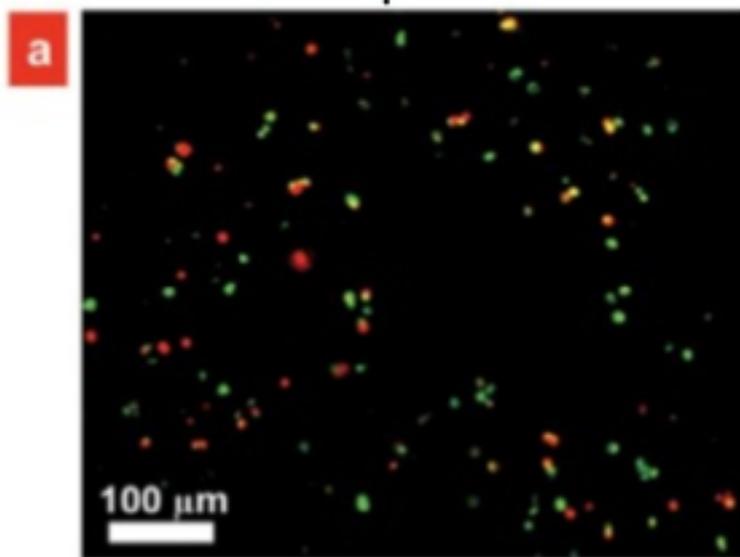


Freedom for modification:

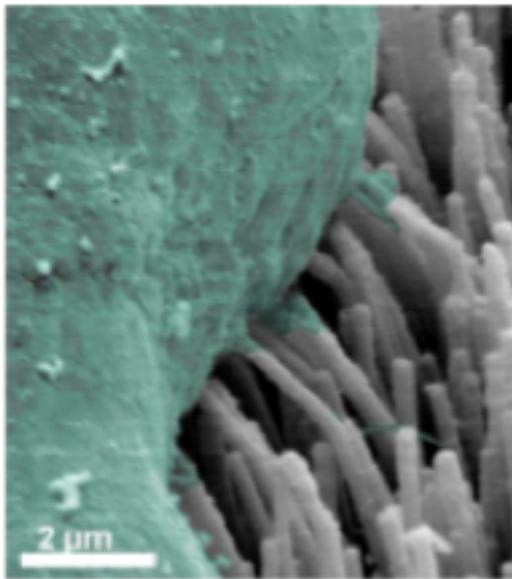
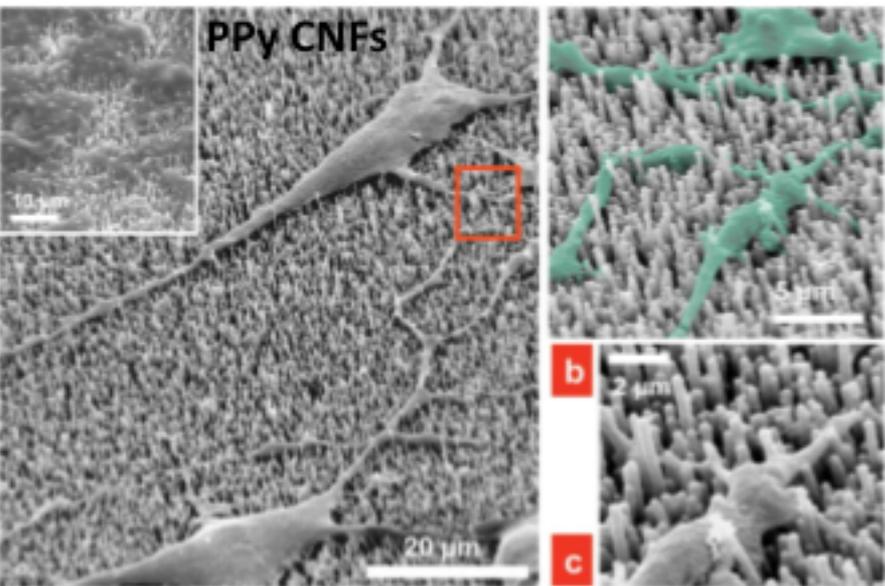
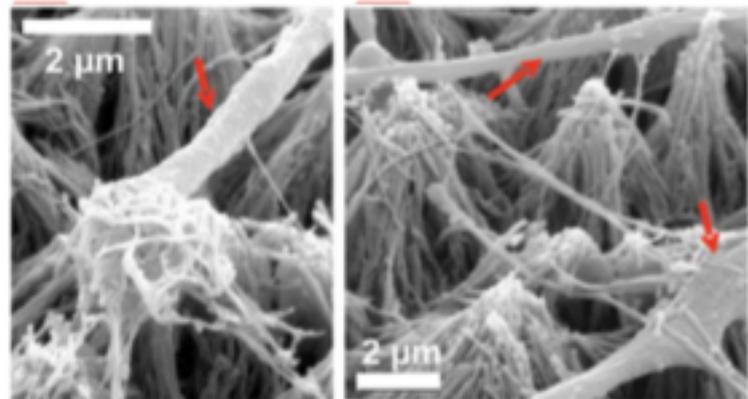
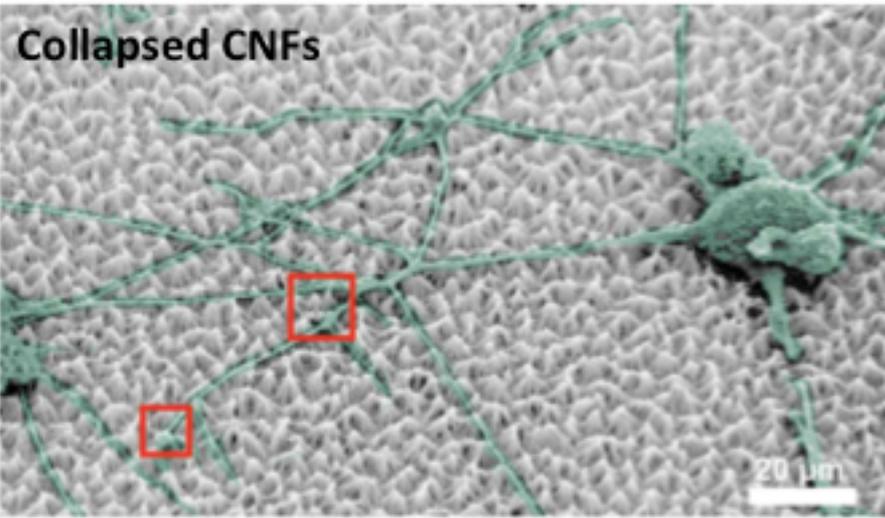
- (1) Changing anion dopants such as Cl<sup>-</sup>, ClO<sub>4</sub><sup>-</sup>, poly(styrenesulfonate) (PSS), other polyelectrolytes, etc.
- (2) Loading with drugs such as antibiotics, anti-inflammatory molecules, etc. and biomolecules such as nerve growth factors.
- (3) Surface functionalization with cell adhesion molecules and specific ligands.

Cl<sup>-</sup> dopant

PSS dopant



# PC12 cells on PPy coated CNFs



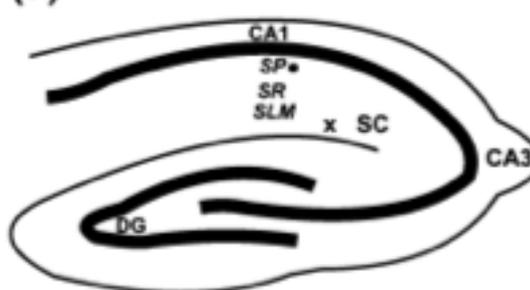
# Stimulation of Rat Hippocampal Brain Slices

**Experiment:** Measure voltage for a given stimulation current

Stimulation by:

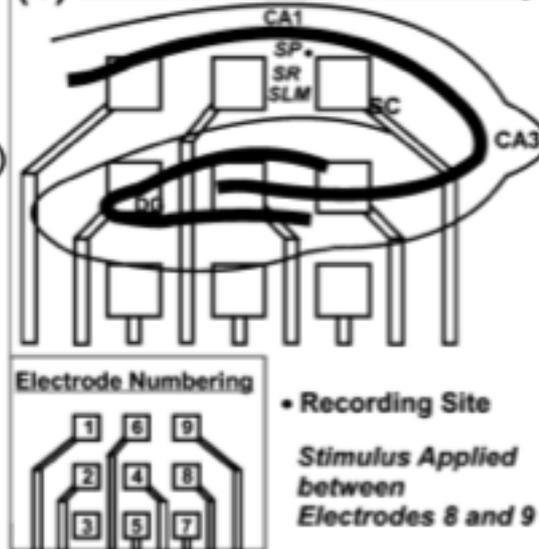
- W wire
- ◆ Pt Microelectrode
- ◆ CNFs
- ◆ PPy coated CNFs

(a) Tungsten Electrode Stimulation

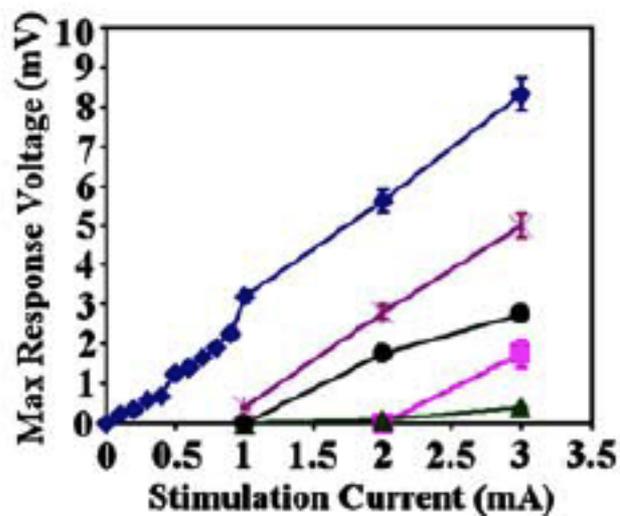


• Recording Site  
x Stimulation Site

(b) Slice Placement on Electrode Array



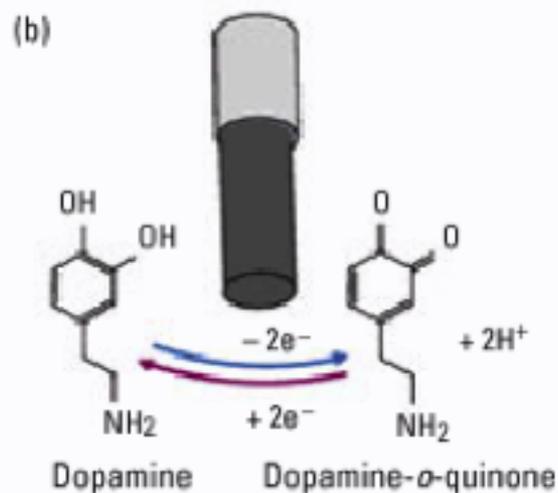
• Recording Site  
Stimulus Applied between Electrodes 8 and 9



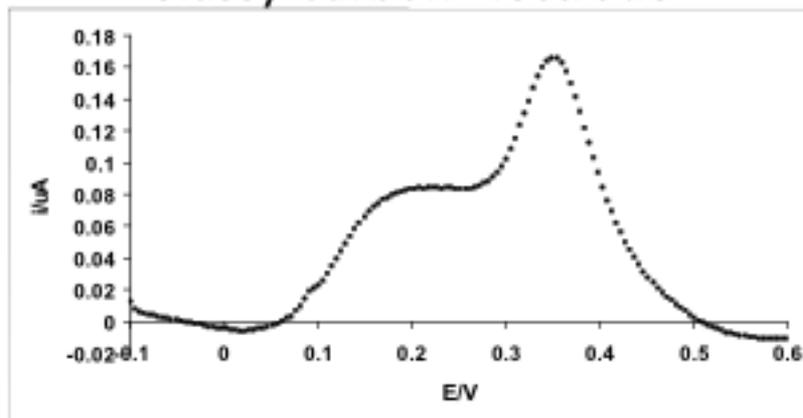
- 1) Only PPy coated CNFs were able to stimulate tissue under 1 mA stimulation current.
- 2) Only PPy coated CNFs did not induce the electrolysis of water (less than 1 mA and 1V)

# Electrochemical Detection of Neurotransmitters

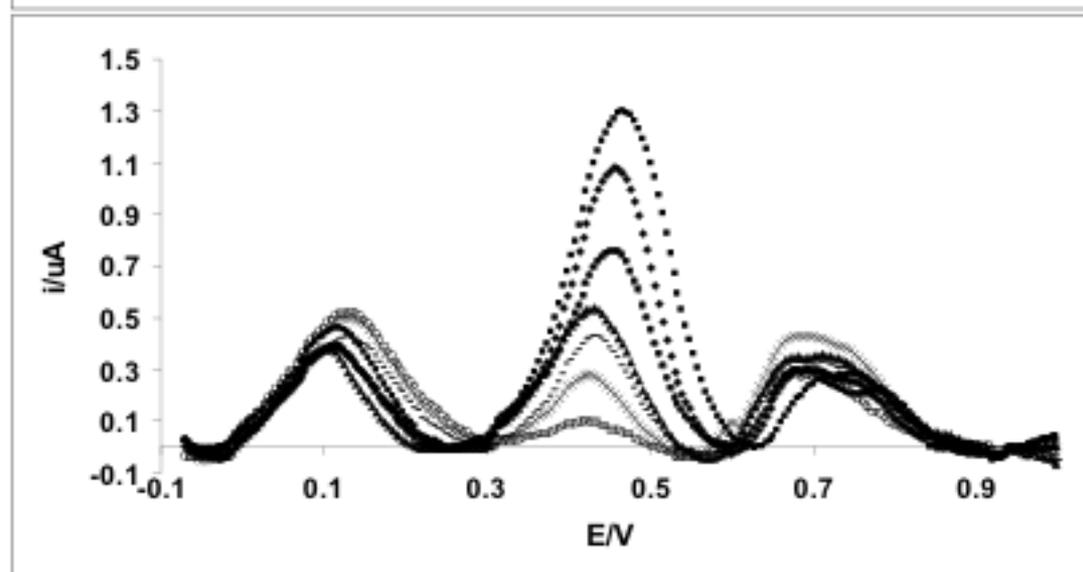
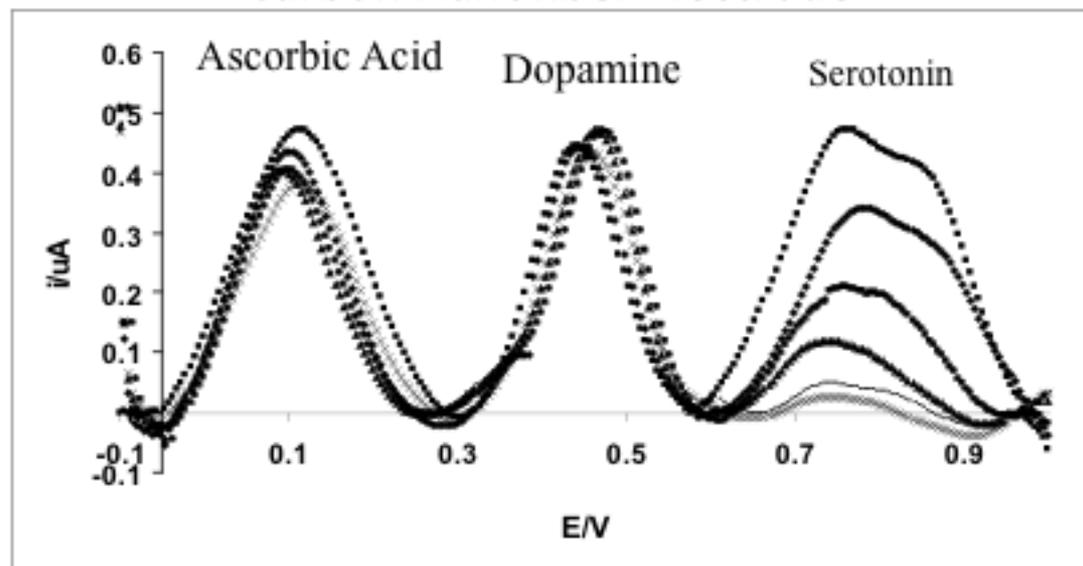
- Molecules of Interest
  - Dopamine
    - Movement disorders, addiction
  - Serotonin
    - Depression, hunger
  - Adenosine
  - Oxygen
  - Hydrogen Ions (pH)
- Techniques
  - Differential Pulse Voltammetry
    - More sensitive
  - Fast Scan Cyclic Voltammetry
    - Better temporal resolution



## Glassy Carbon Electrode



## Carbon Nanofiber Electrode



-CNF electrode has ability to distinguish multiple electroactive brain chemicals in a mixture!  
-Detection limits 50nM for DA and 100nM for 5-HT

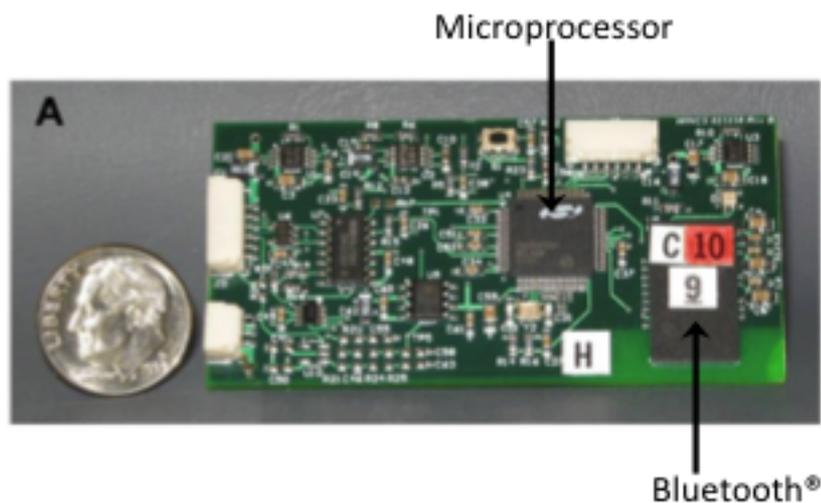
# Wireless Instantaneous Neurotransmitter Concentration Sensor (WINCS)

The Mayo Clinic-developed WINCS is a microprocessor-controlled, MRI-compatible, battery-powered instrument that combines Bluetooth® digital telemetry with fast scan cyclic voltammetry and constant potential amperometry.

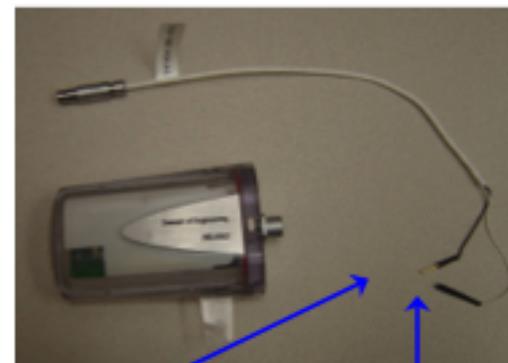
Standard Potentiostat



Printed Circuit Board



Sterilizable WINCS Unit



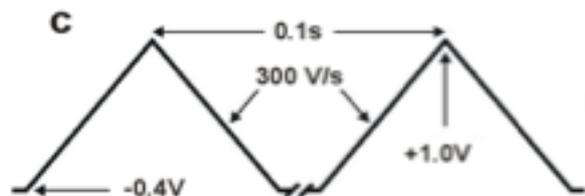
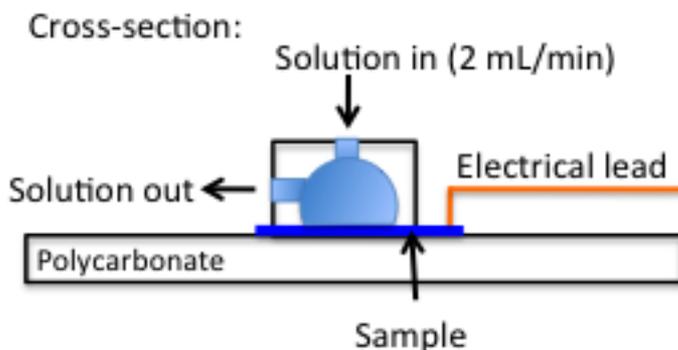
Reference Electrode Lead

Working Electrode Lead

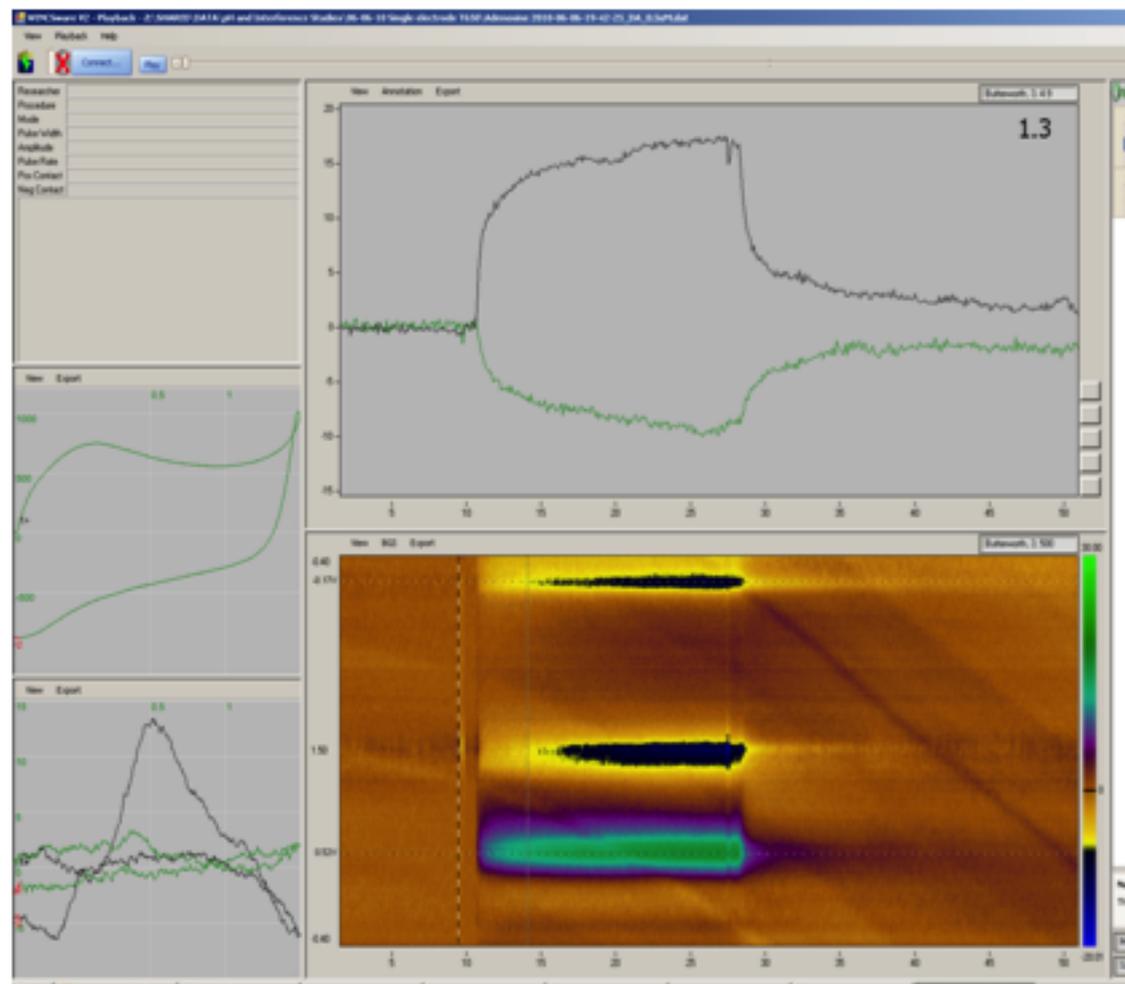
**WINCS was designed in compliance with FDA-recognized standards for medical electrical device safety.**

# Experimental Setup

Custom-Designed Flow Cell

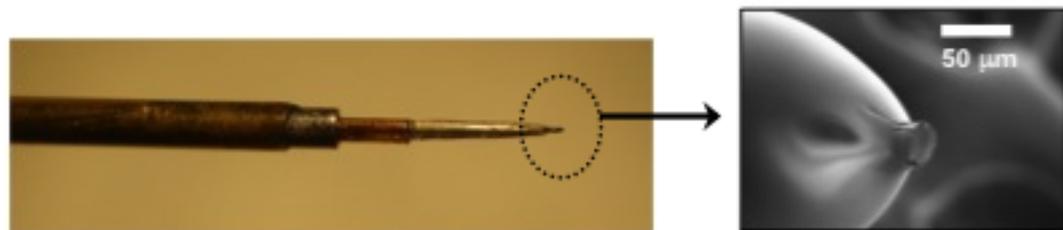


WINCSware User Interface



**WINCSware allows viewing of the data in nearly real-time**

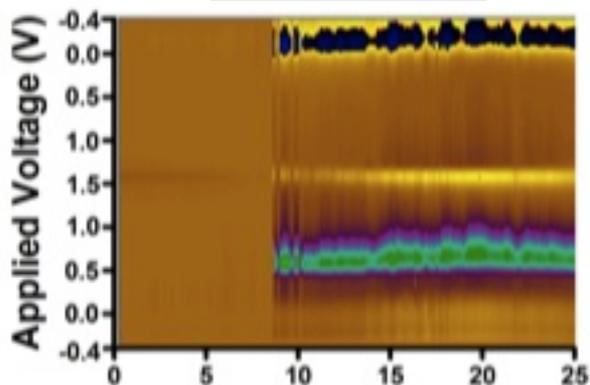
# WINCStroke for the Detection of Dopamine



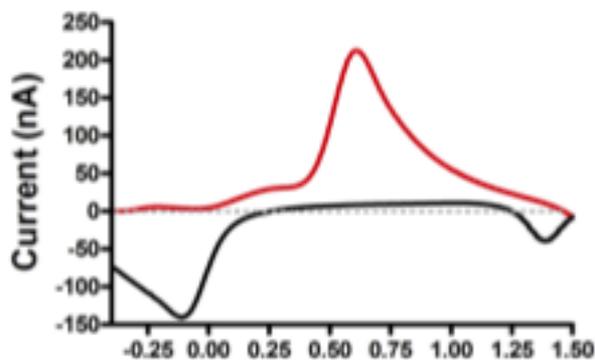
The WINCS carbon fiber electrode (WINCStroke) is based on an approved human extracellular tungsten electrophysiology electrode that was modified by the addition of a short section of carbon-fiber to enable FSCV recordings.

## Dopamine Detection:

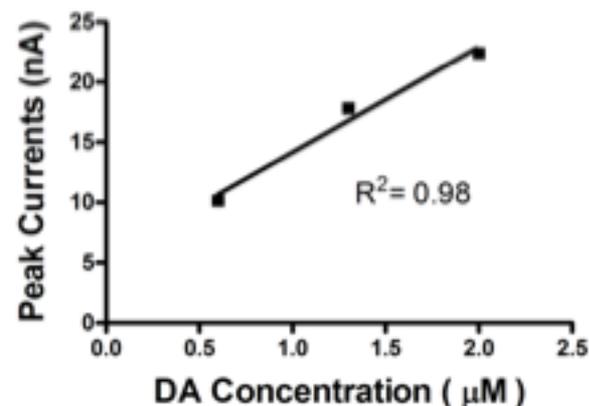
### 3D Color Plots



### Background Subtracted Cyclic Voltammogram

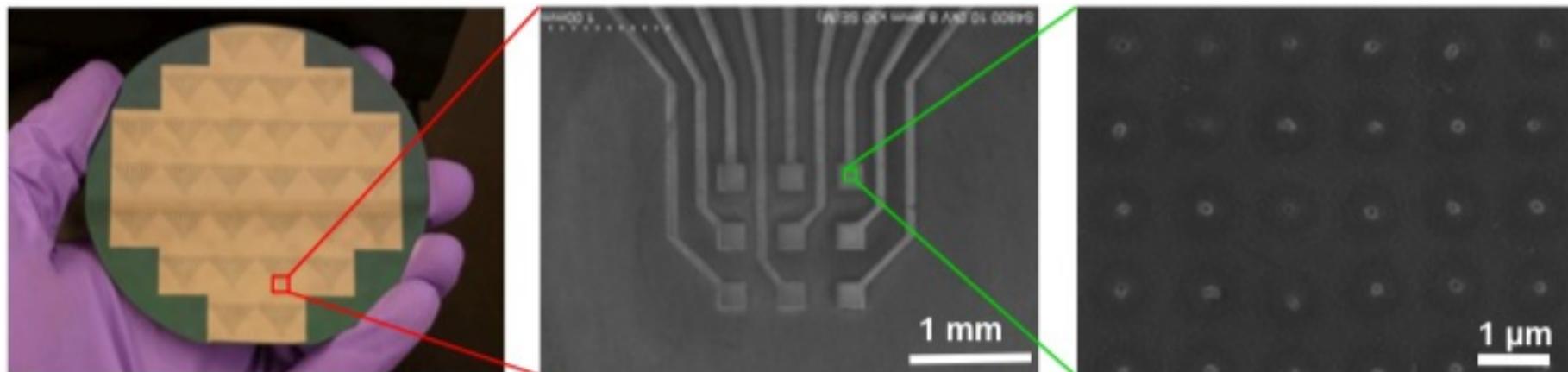


### Calibration Curve

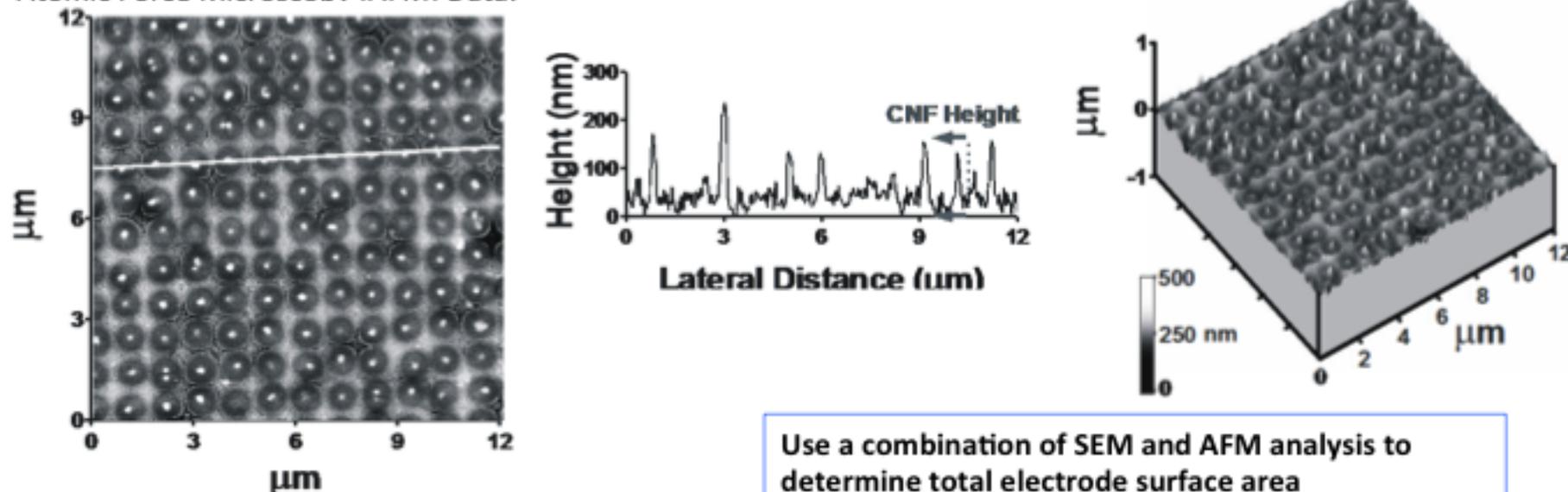


# WINCS Carbon Nanofiber Electrode (WINCSnanotrode)

Scanning Electron Microscopy (SEM) Data:



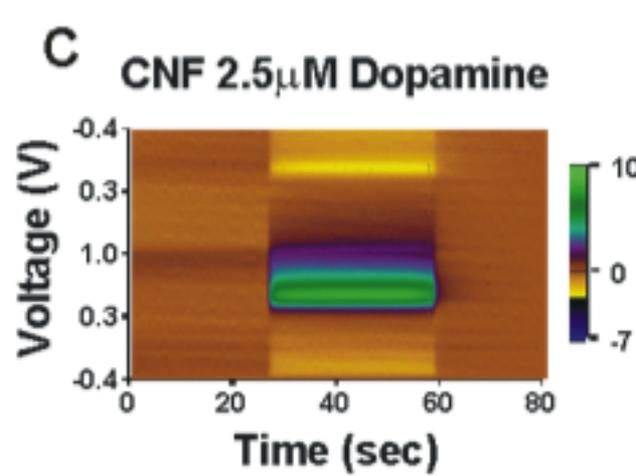
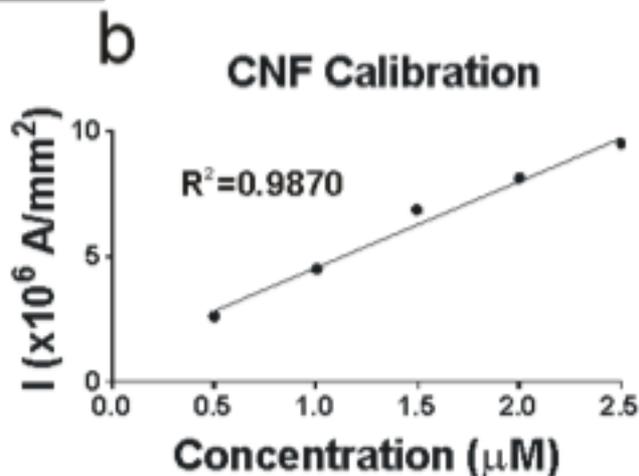
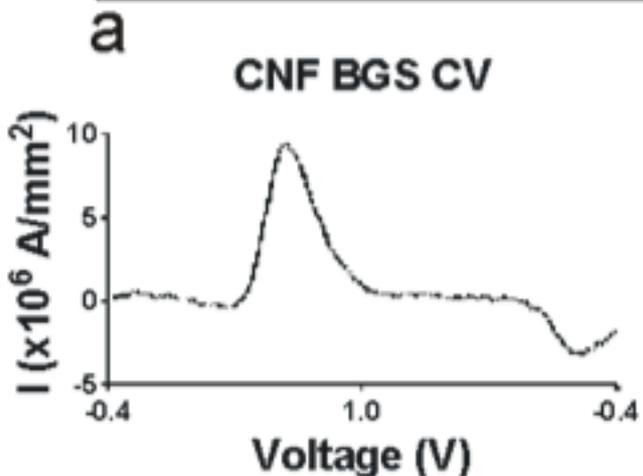
Atomic Force Microscopy (AFM) Data:



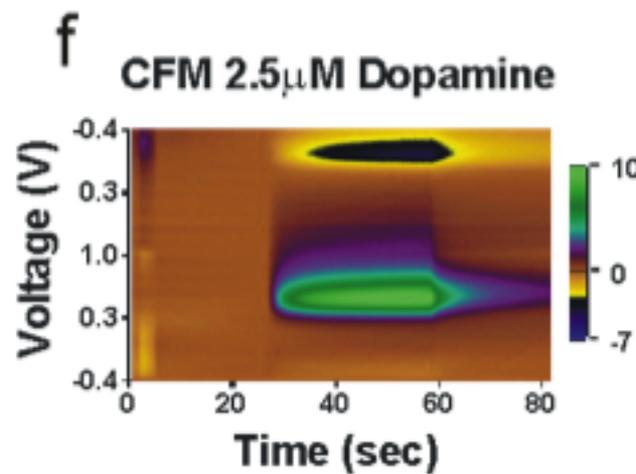
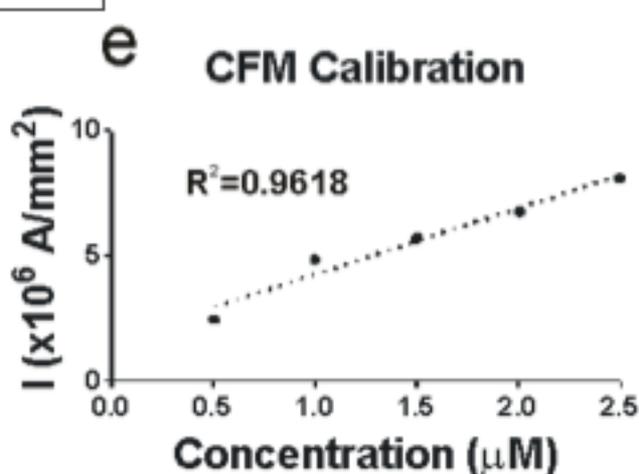
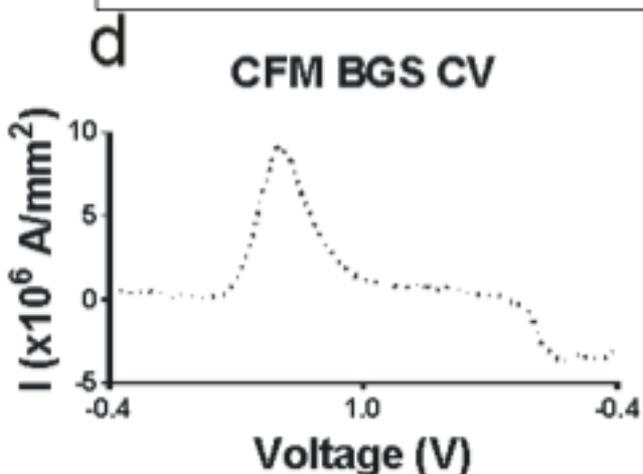
Use a combination of SEM and AFM analysis to determine total electrode surface area

# Dopamine Detection

## Carbon Nanofiber Electrode



## Carbon Fiber Microelectrode

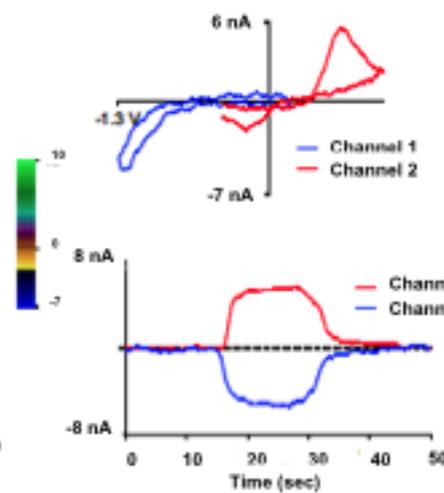
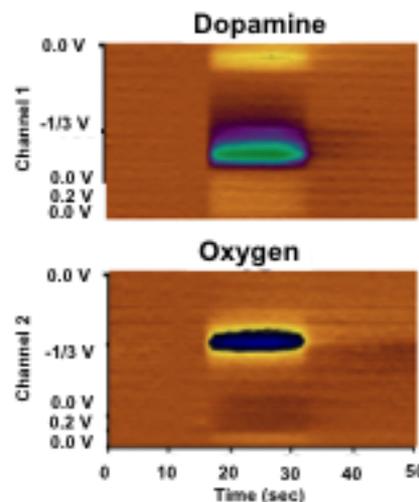
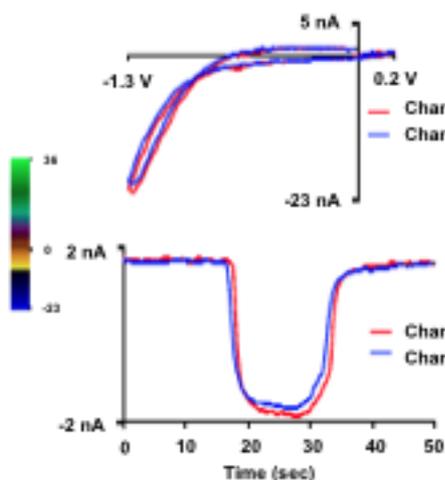
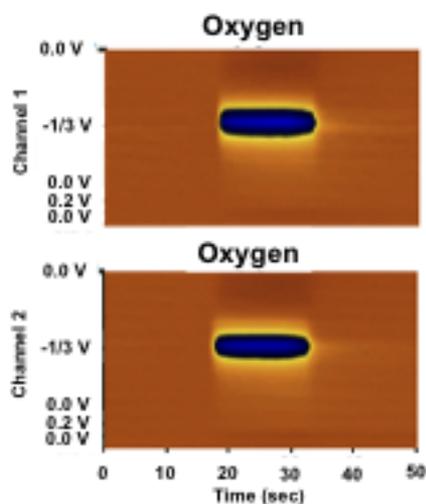
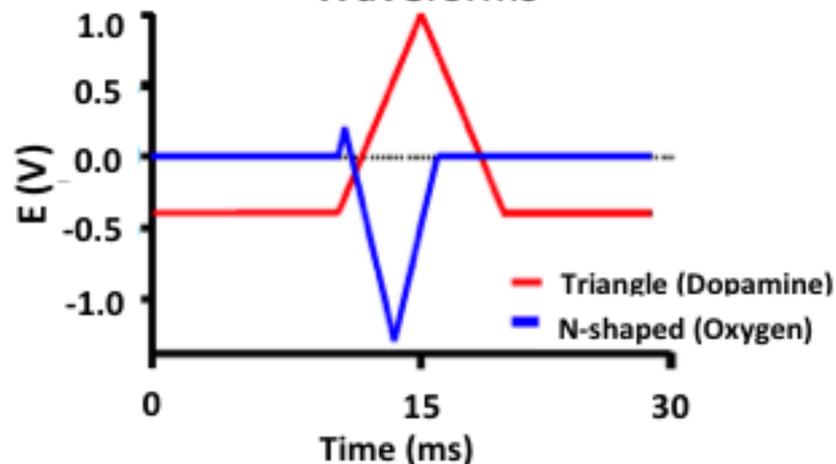
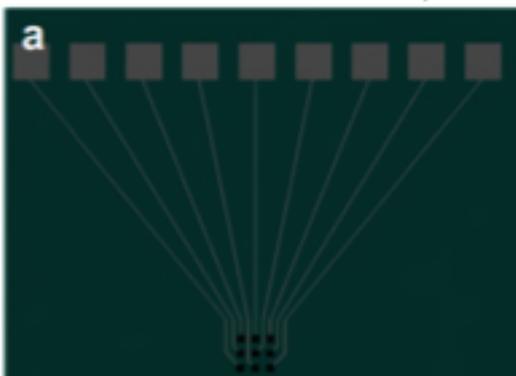


# Multichannel Recording

Device: 3x3 Array

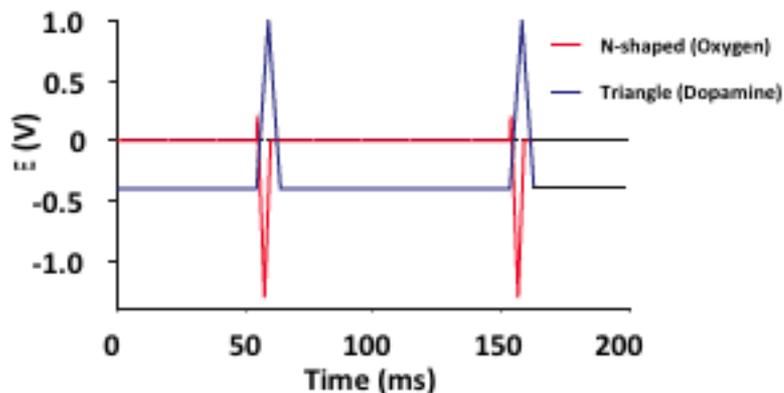
Instruments: 2 WINCS

Waveforms

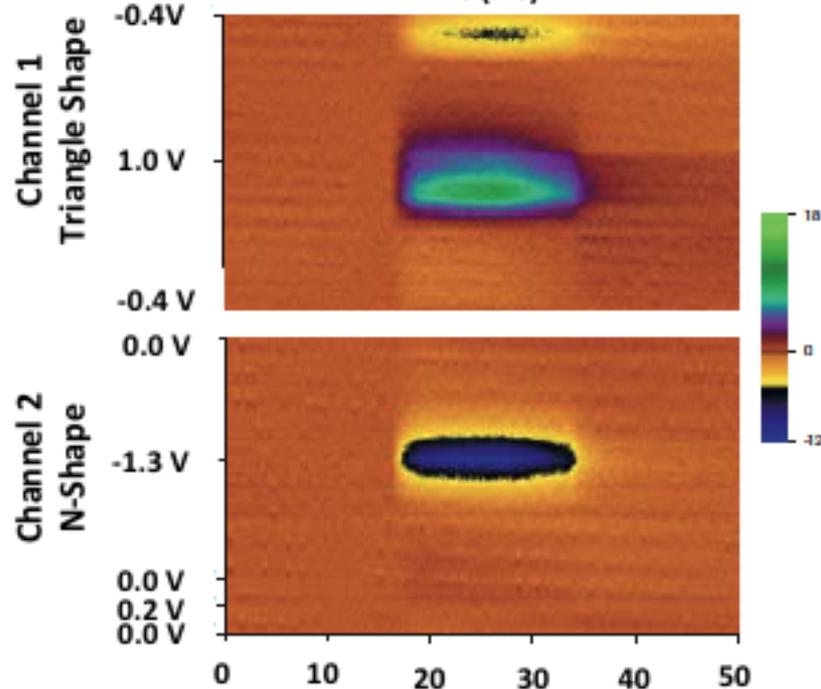
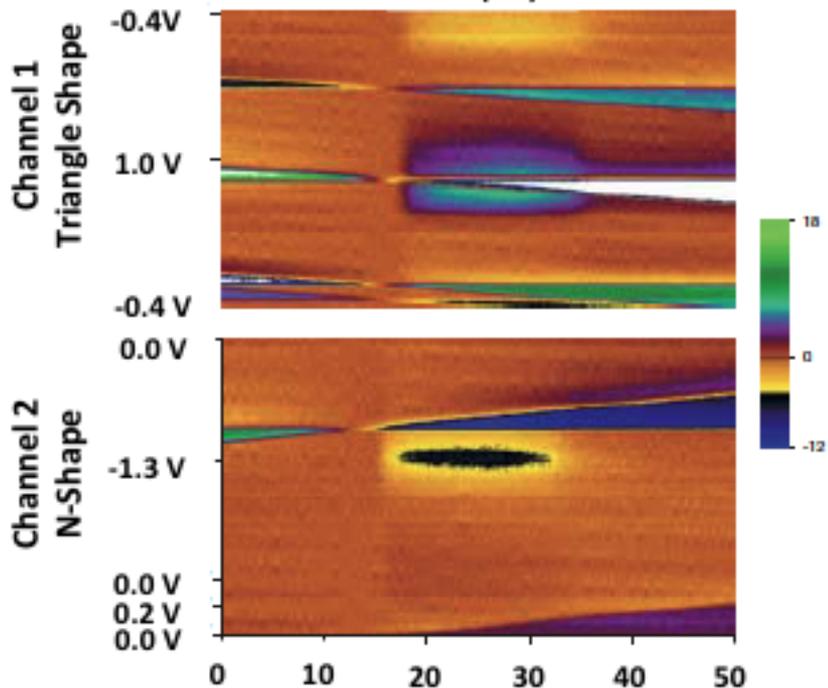
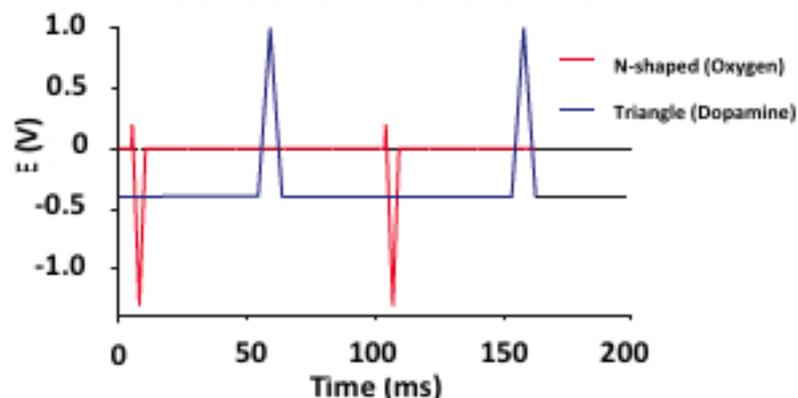


# Multichannel Crosstalk

Overlapped Waveforms



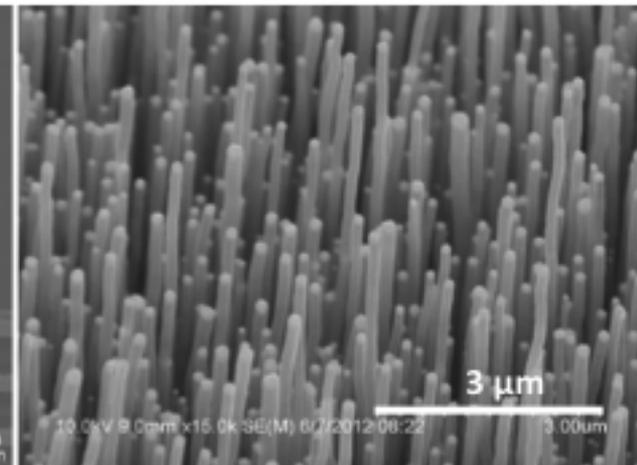
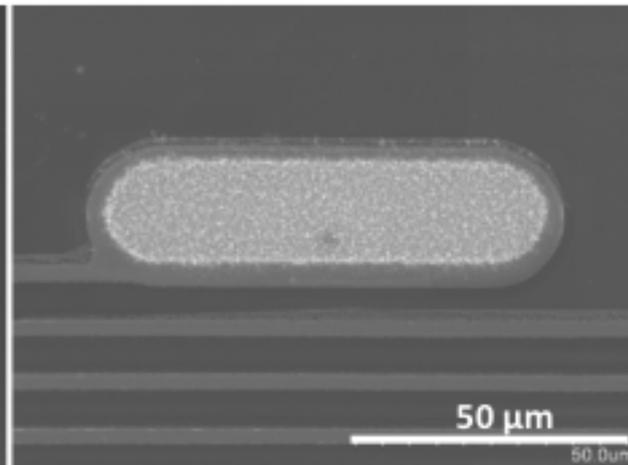
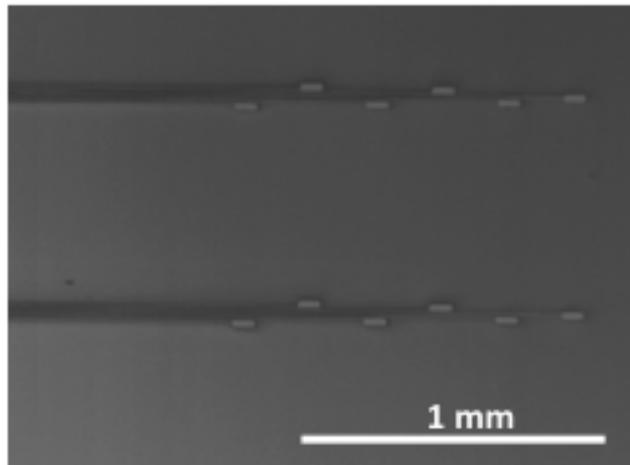
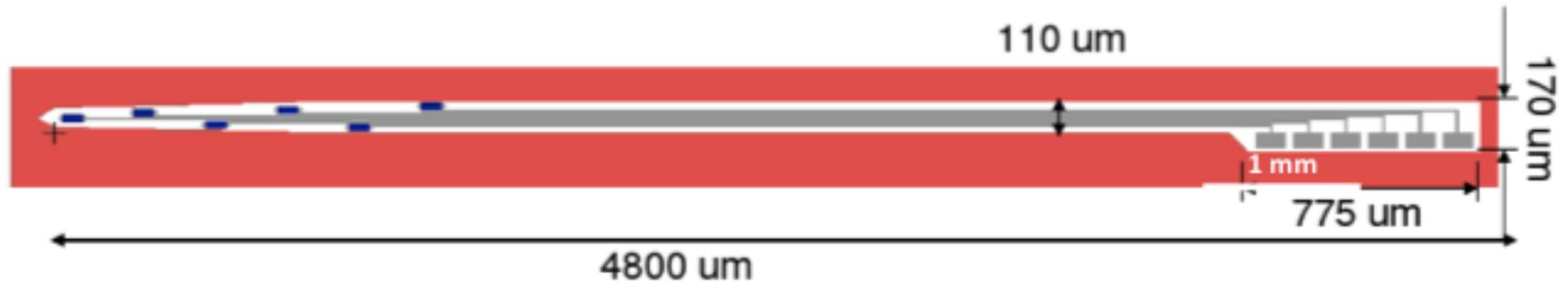
Interleaved Waveforms



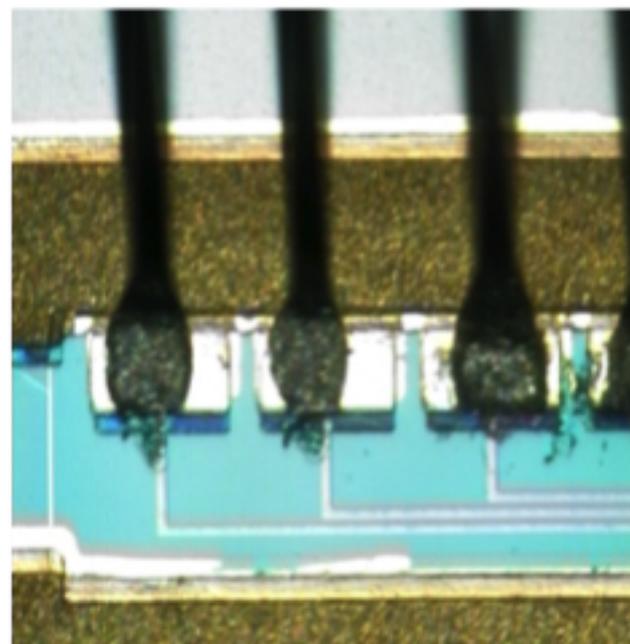
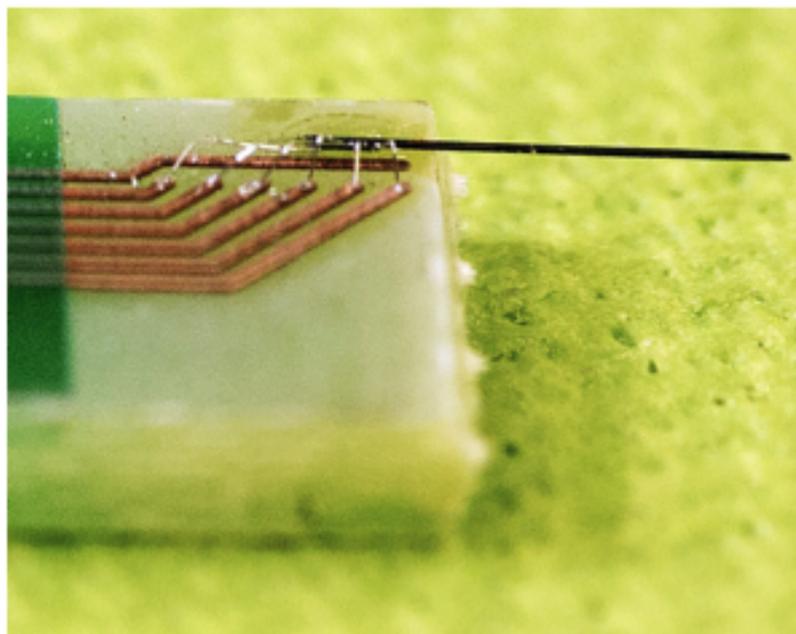
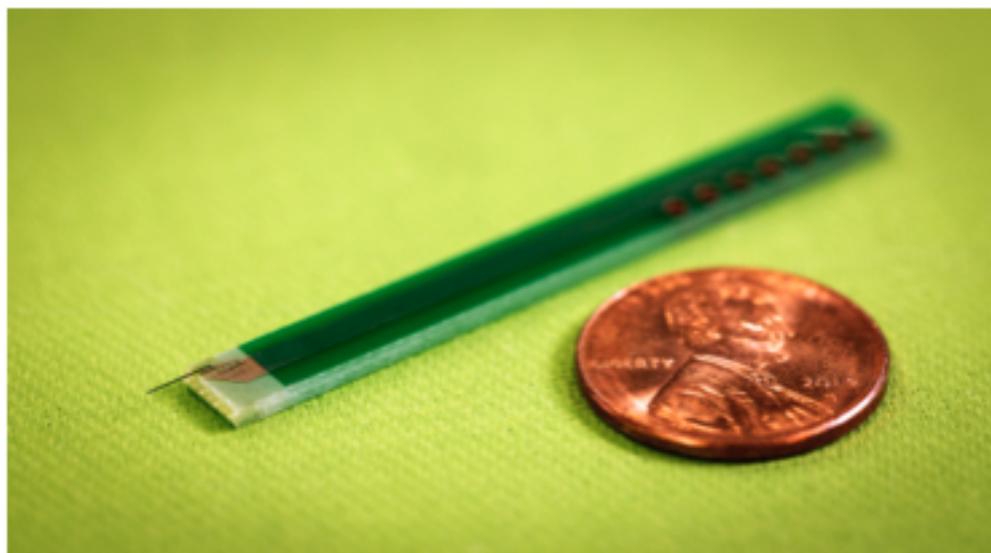
## Implantable Style CNF Electrode Needle

Penetrating multiplexed array

- Ability to spatially resolve

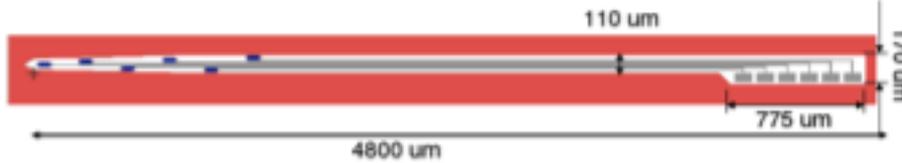


# Needle Assembly

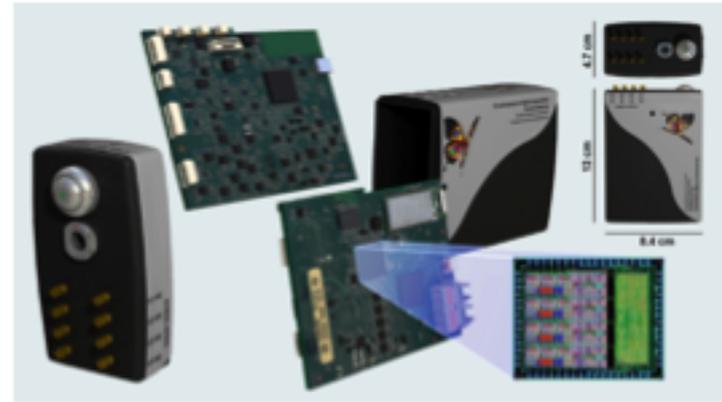


# Simultaneous Multichannel Oxygen Detection

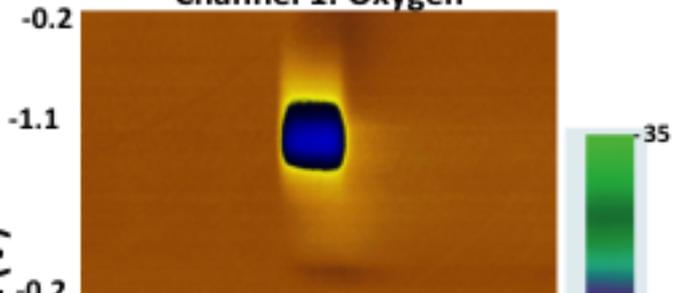
Device: Needle



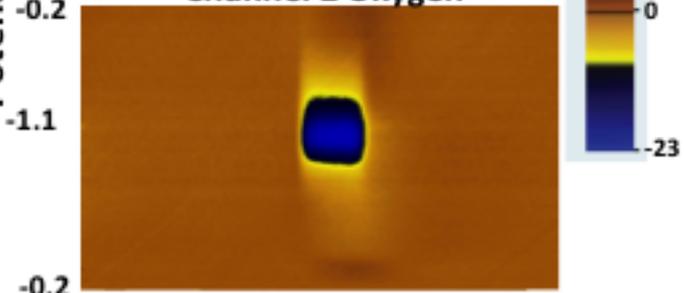
Instrument: WINCS Harmoni



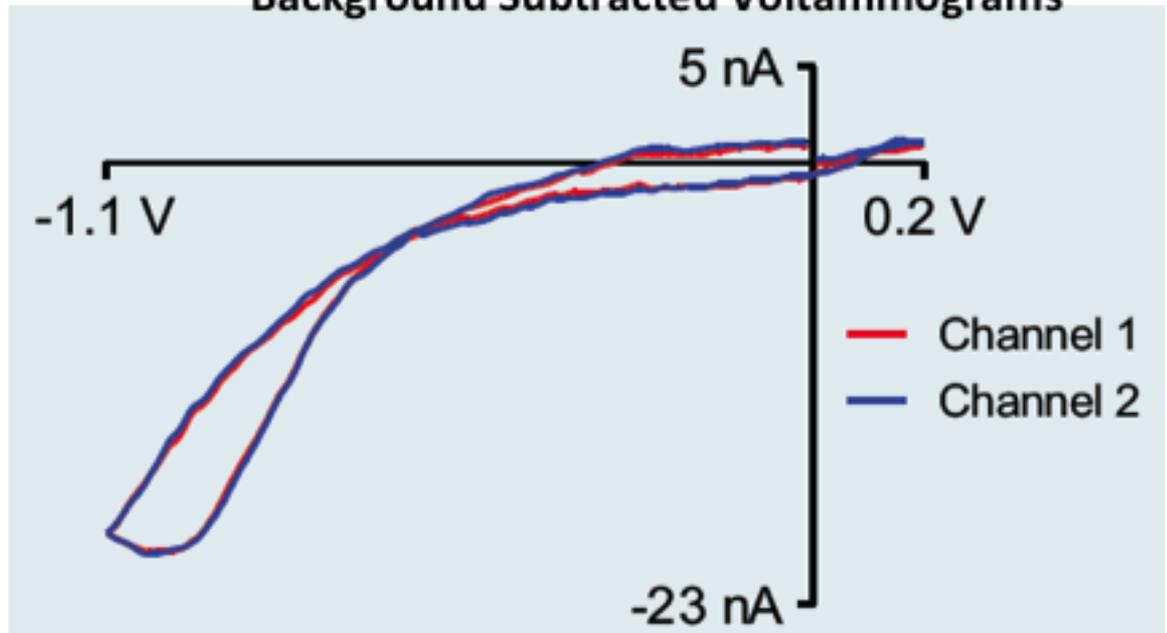
Channel 1: Oxygen



Channel 2 Oxygen

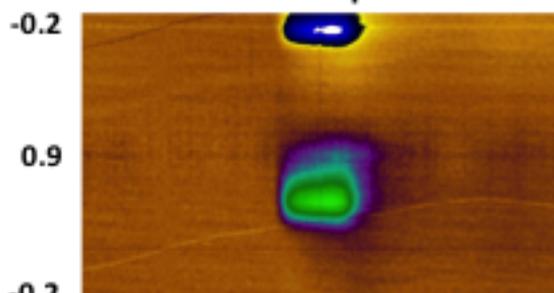


Background Subtracted Voltammograms

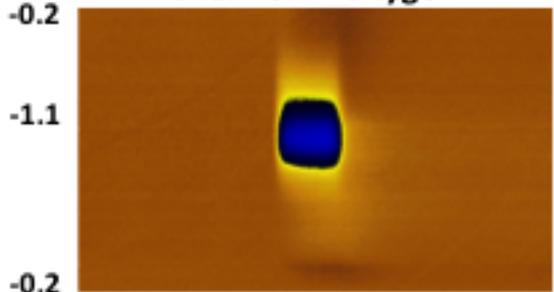


# Multichannel Detection: Dopamine and Oxygen

Channel 1: Dopamine

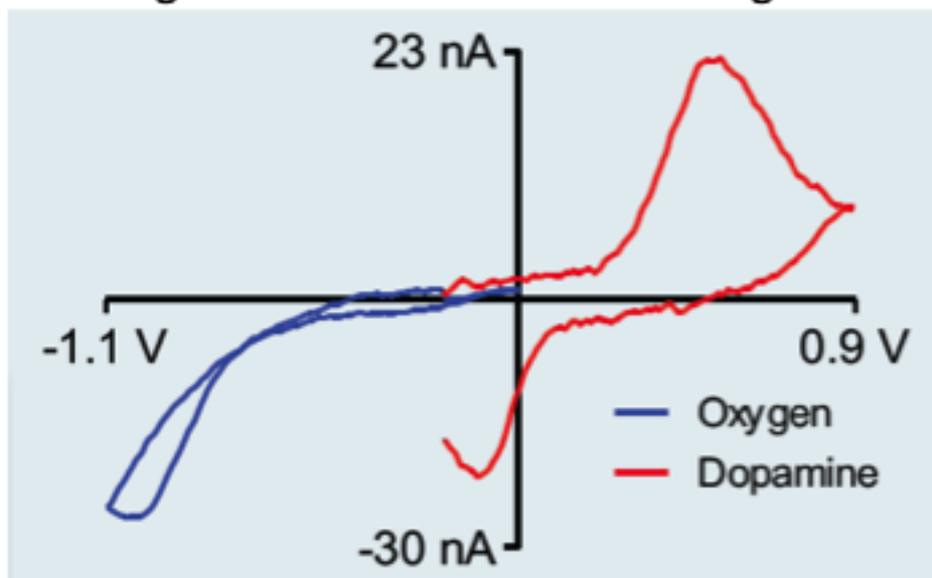


Channel 2: Oxygen

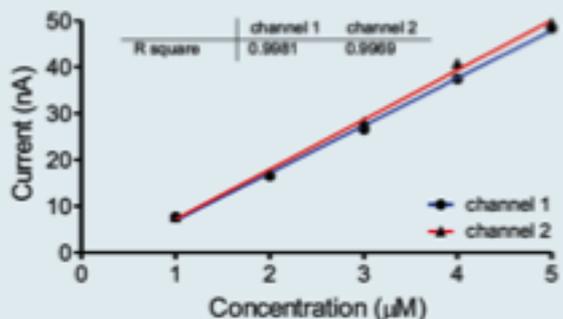


0 10 20 30 40 50  
time

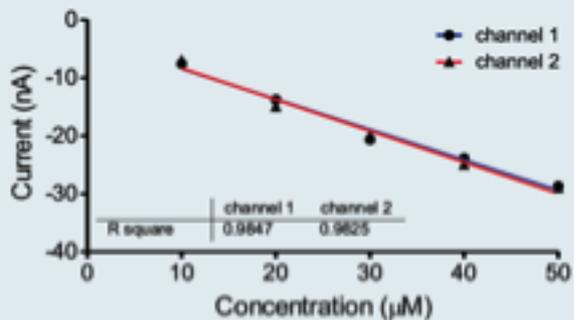
Background Subtracted Voltammograms



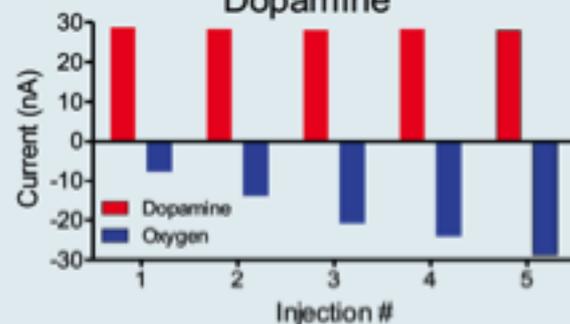
Dopamine Calibration



Oxygen Calibration



Increasing Oxygen with Constant Dopamine



# Summary

- Carbon nanofiber nanoelectrode arrays are easily fabricated using standard silicon processing
  - CNF spacing defined by photolithography, e-beam lithography or top layer dielectric polishing time
- High surface area carbon nanofibers have been demonstrated as effective stimulation electrodes
- Conductive polymer coatings have allowed us to tune the electrical properties and biocompatibility
- CNF sensors can distinguish between multiple electroactive analytes in a mixture using differential pulse voltammetry
- CNFs nanoelectrode arrays easily integrate with WINCS
- CNFs detect dopamine and oxygen with no channel cross-talk
- We have successfully fabricated a needle-like, implantable CNF electrode array for future in vivo investigations

# Acknowledgements

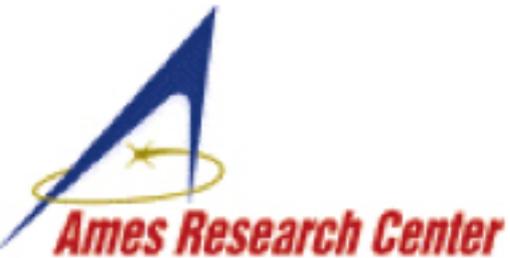
- NASA Ames Research Center
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  - Adwoa Boakye
  - Brandon Douglas
  - **Russell J. Andrews**
  - **M. Meyyappan**
- Mayo Clinic
  - Department of Physiology and Bioengineering
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    - Su-youne Chang
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  - Department of Engineering
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